

# Metabolic Seminar – 23<sup>rd</sup> of January 2013

Institute of Physiology AS ČR, p.r.i.

## $\mu$ PET/CT

Molecular imaging in small laboratory animals



# Molecular Imaging



*In vivo* molecular imaging in small animals is the bridge between *in vitro* data and translation to clinical application

Multiple longitudinal images provide more reliable information and reduce animal numbers

Discover new predictive imaging biomarkers

Accelerate the pre-clinical validation of new drugs

Enable selection of drug candidates for clinical translation

**No one imaging method is ideal for all studies**

# Morphological Imaging

## CT

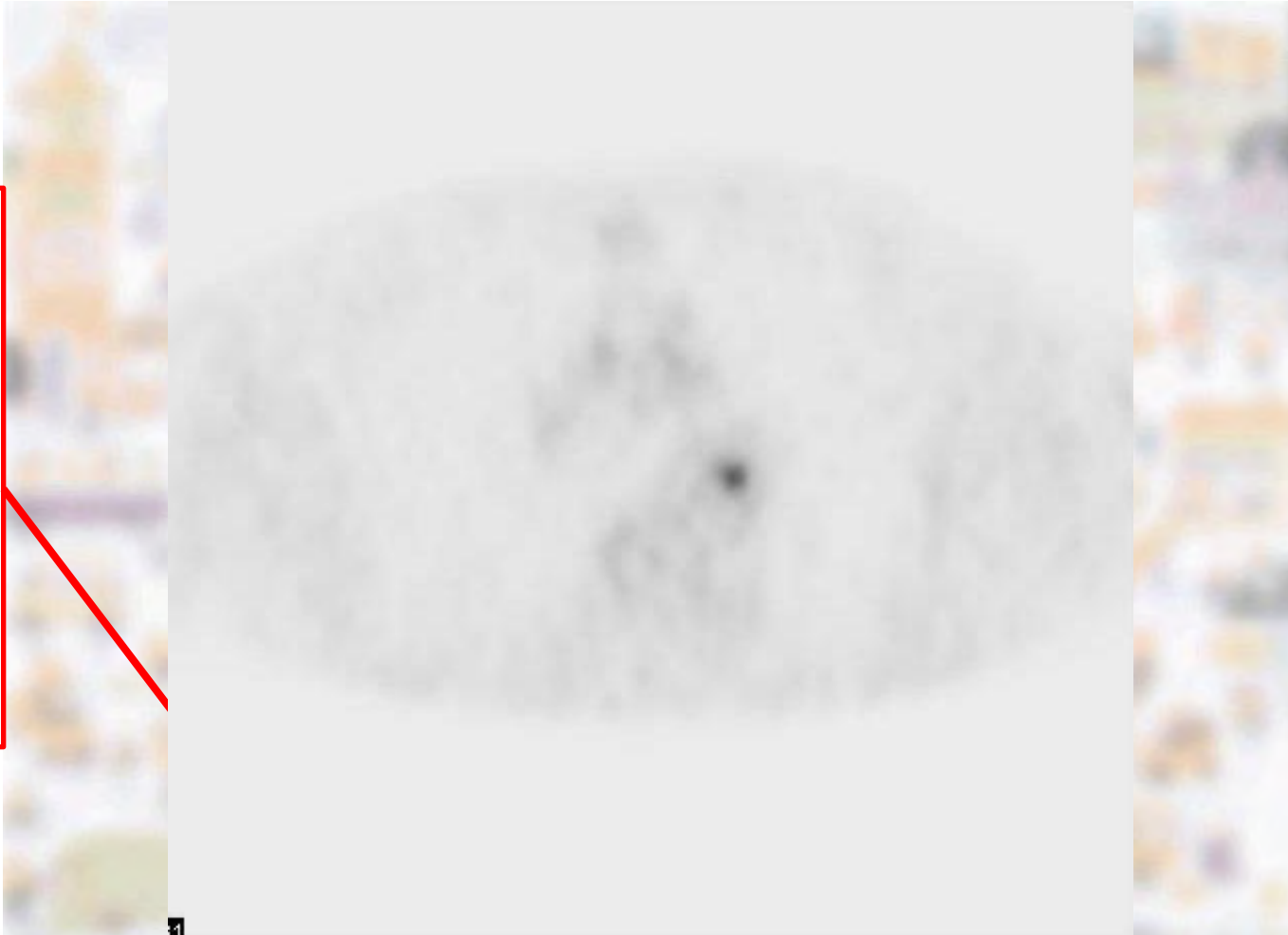


Out of: Richard Scarry's Children's Books



# Functional Imaging

## PET

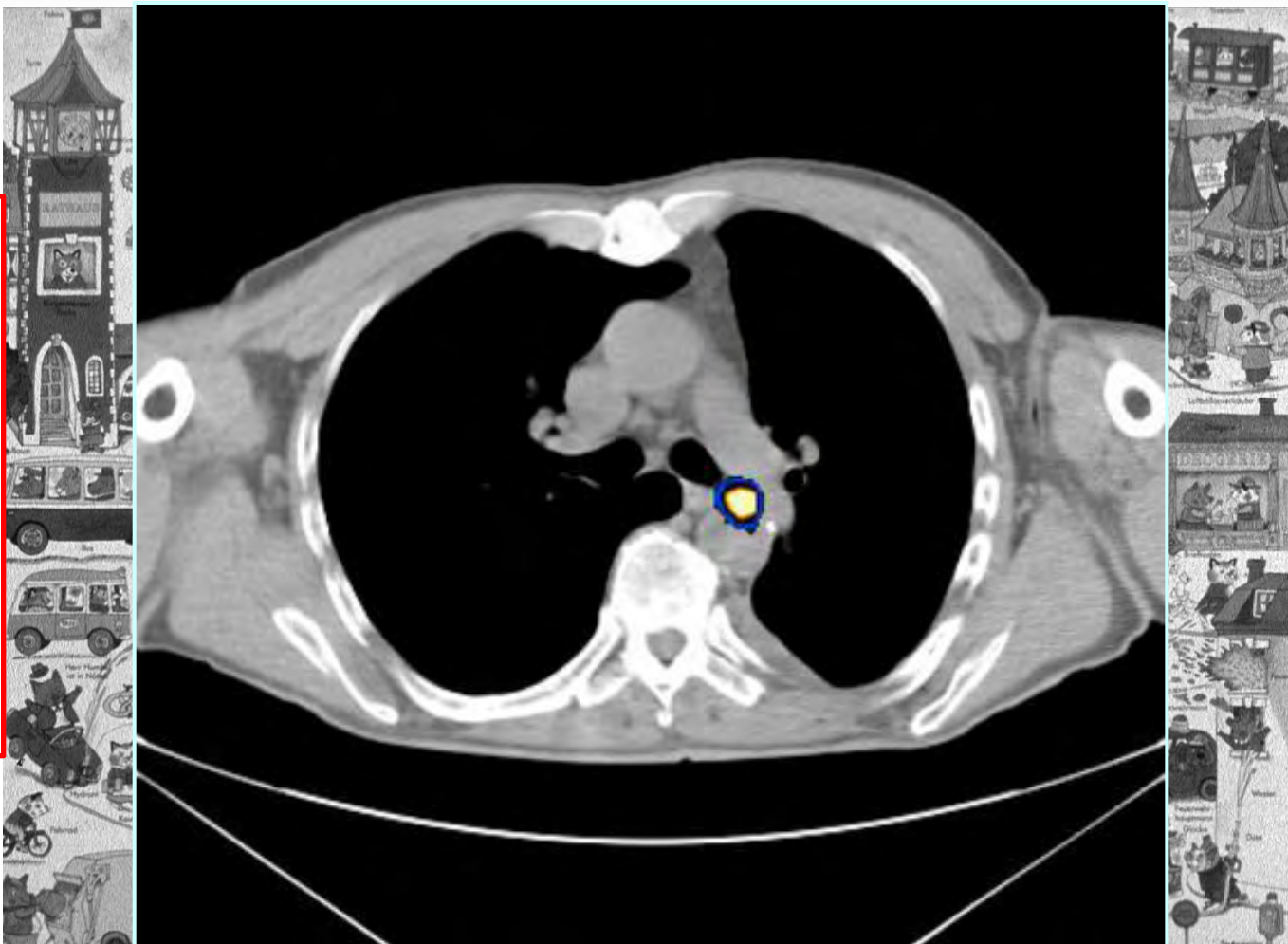


Out of: Richard Scarry's Children's Books



# Image Fusion

## PET/CT



Out of: Richard Scarry's Children's Books



# *In vivo* biomedical imaging technologies

Anatomic

Physiologic

Metabolic

Molecular

**optical imaging**

**x-ray CT**

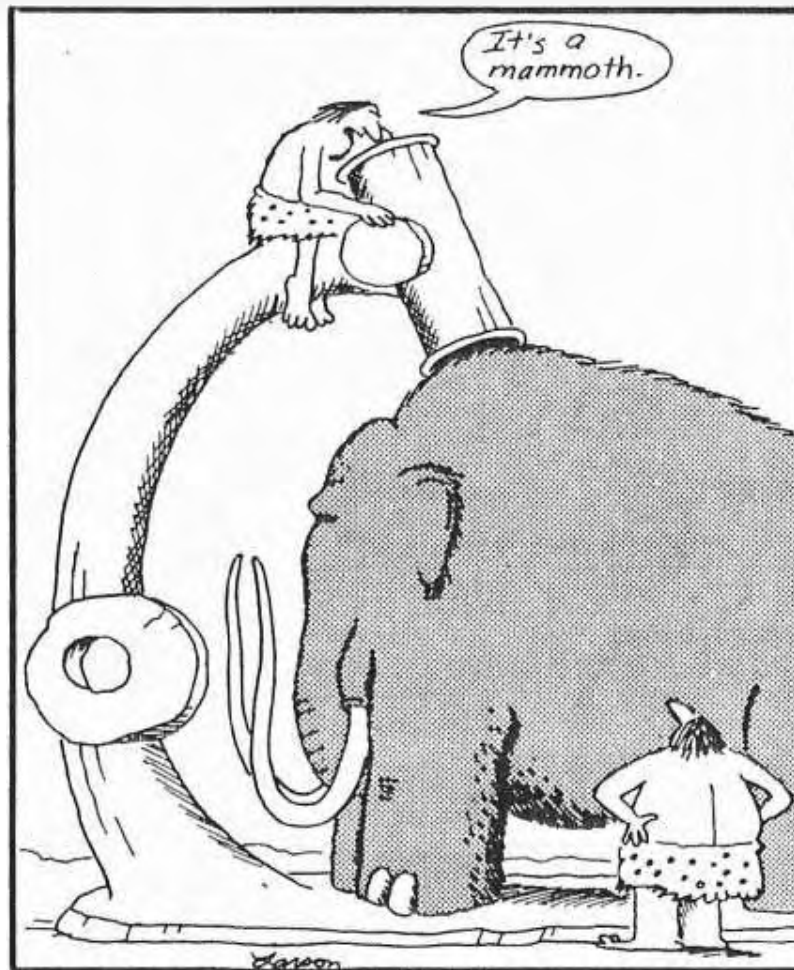
**PET/SPECT**

**MRI**

**ultrasound**



# Molecular Imaging: The Big Picture

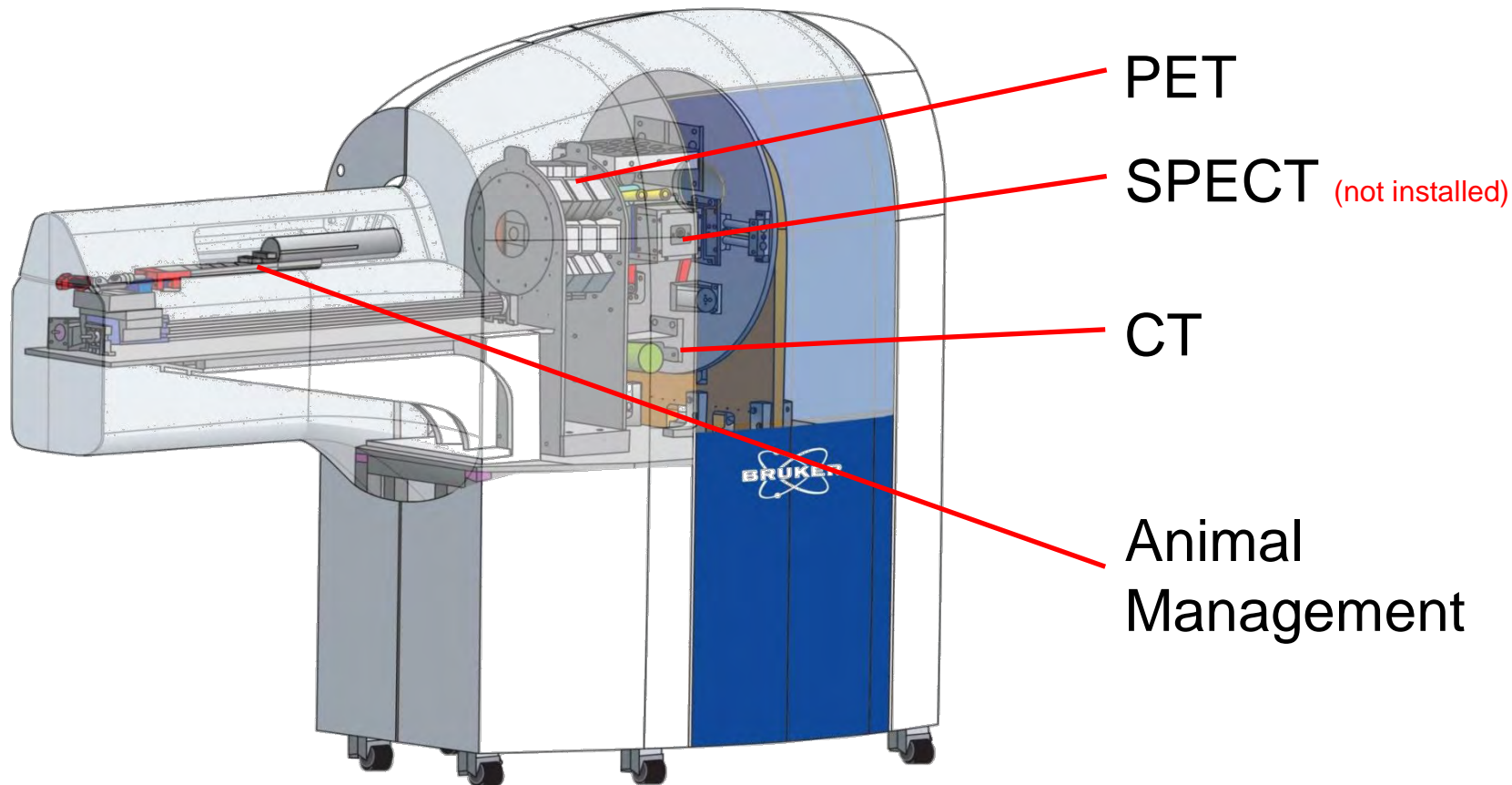


Early Microscope



# Albira

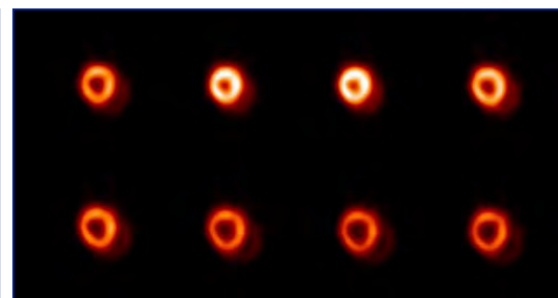
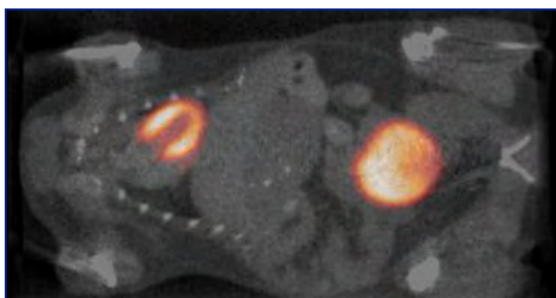
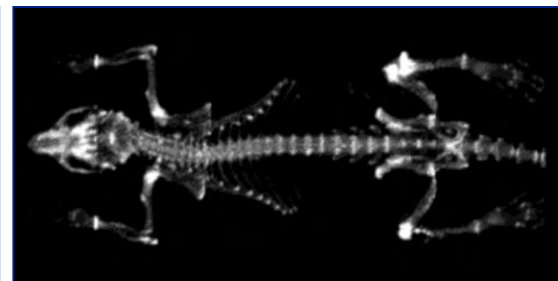
PET/SPECT/CT





# Small Animal Imaging

## Requirements



### High spatial resolution

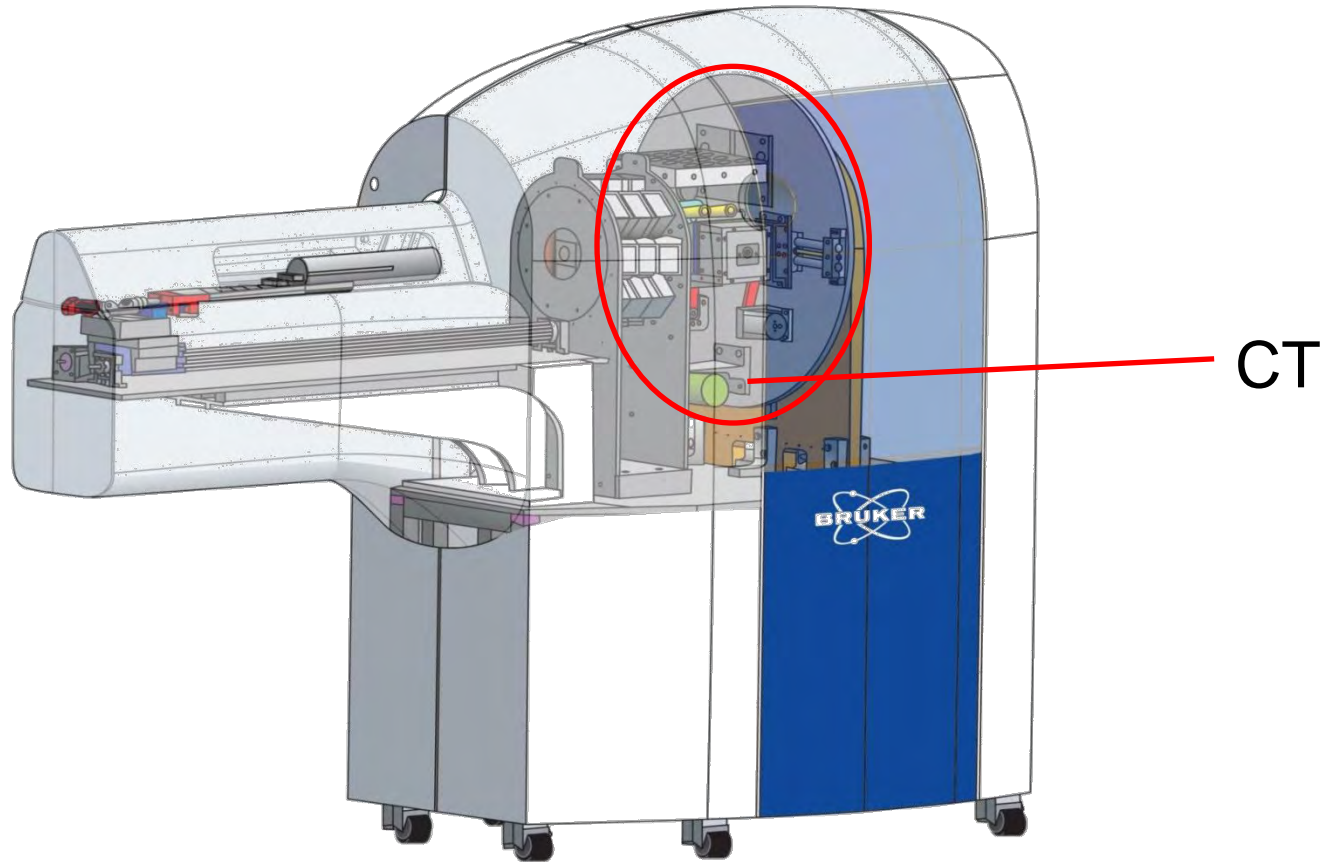
- mouse organs ~1000-fold smaller volume than human

### High sensitivity

- number of targets also smaller, radiation dosimetry can be limiting

# Computed X-ray tomography

## CT



# Computed X-ray tomography

## CT



### ADVANTAGES

- high spatial resolution (20 $\mu$ m)
- easy to operate
- relatively cheap

### DISADVANTAGES

- sensitivity = milli-molar
- No functional information
- High radiation source
- Bad soft tissue contrast
- Contrast agents required to improve soft tissue contrast

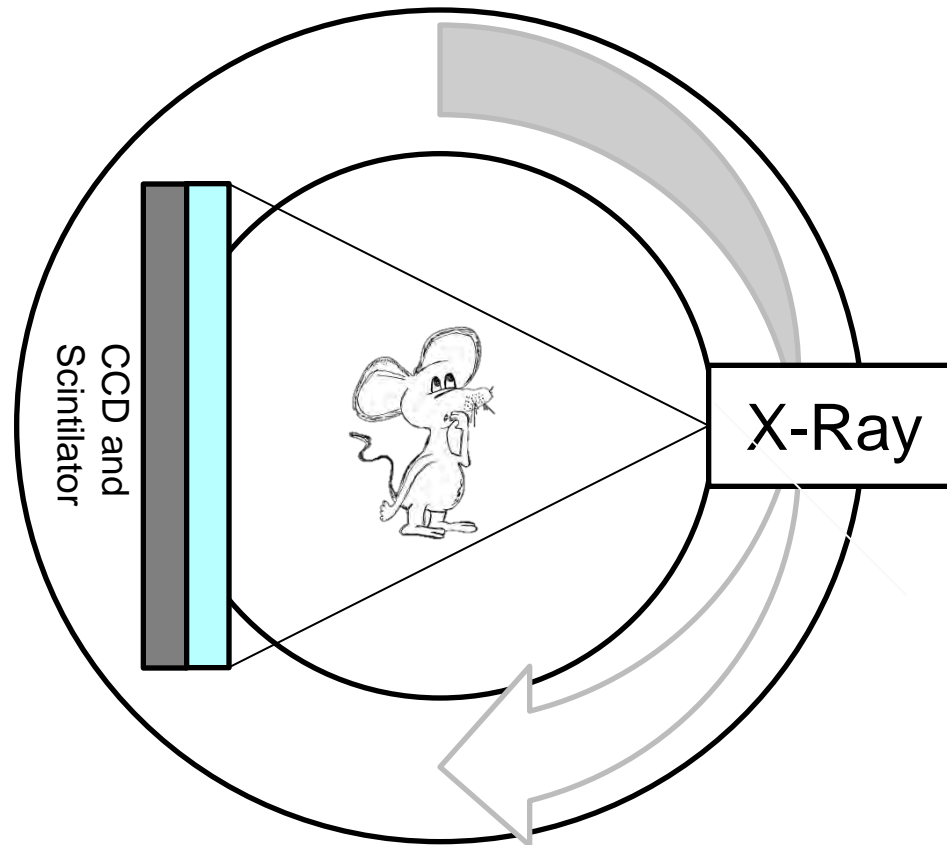
CT is based on the measurement on X-ray attenuation ( $\sim$  40-80 keVp)



# Computed X-ray tomography

## Tomography Principle

X-ray source and X-ray-detector are mounted on a common rotational stage



Projection data are acquired in a **step-and-shoot (SAS) mode**

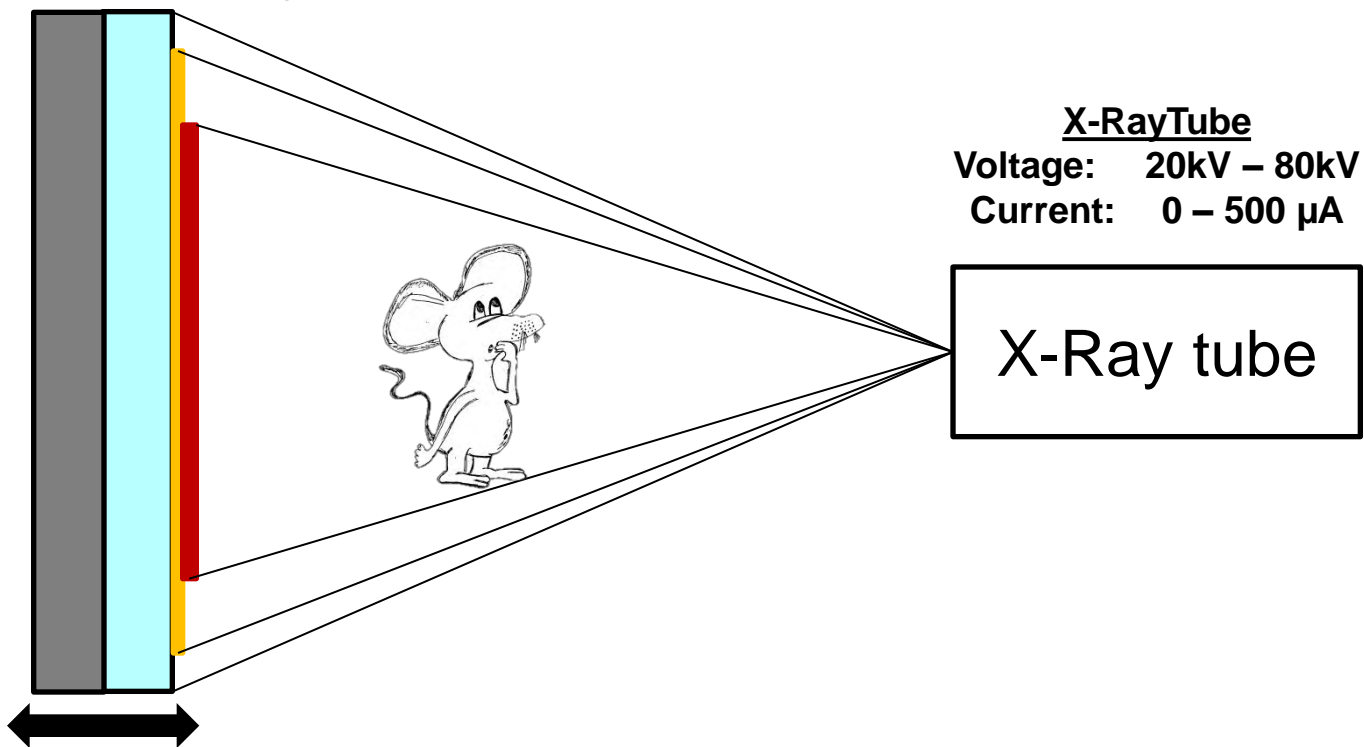
# Computed X-ray tomography

## CT-Detector Principle

### CCD-Array and Scintillator

Scintillator: NaI

CCD Array: Large Area (2048 x 3072, 33microns pitch)



### X-RayTube

Voltage: 20kV – 80kV

Current: 0 – 500  $\mu$ A

X-Ray tube

Move detectorpanel to  
adjust FOV and resolution



# Computed X-ray tomography

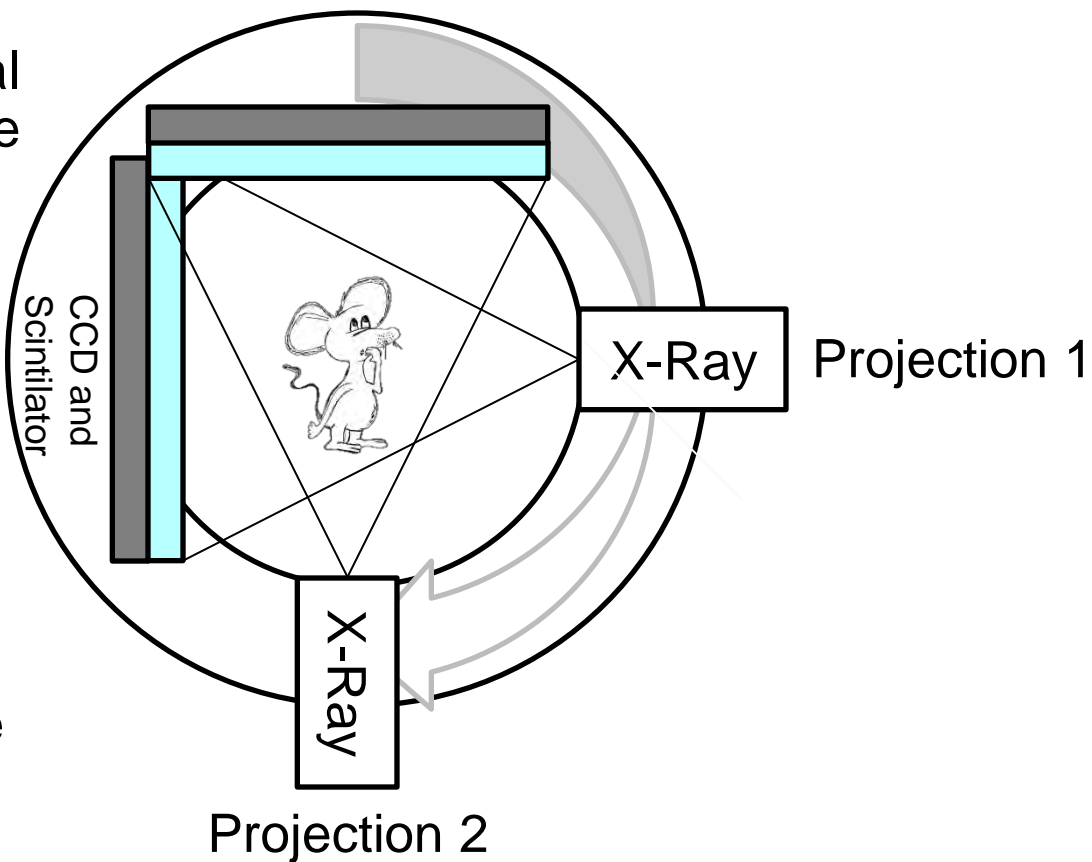
## Step-and-Shoot (SAS) Mode

N projections over an total rotation angel of  $360^\circ$  are acquired

N = number of steps

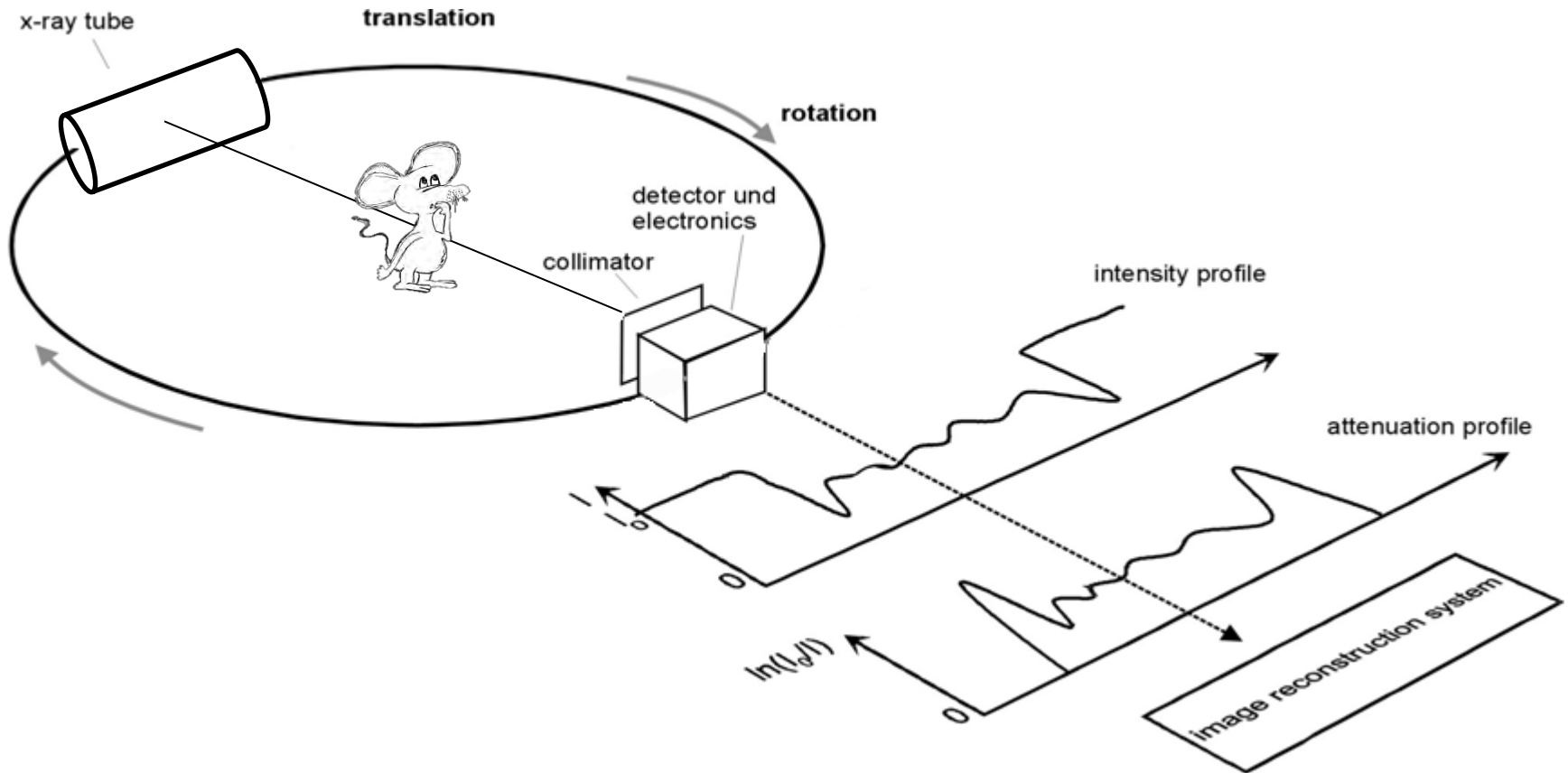
Rotation angle per step depends on preselected resolution

The higher the resolution , the more steps are required



# Computed X-ray tomography

## CT Data Acquisition and Processing



# Computed X-ray tomography

## microCT Reconstruction



No additional sorting process for projection data

→ already sinograms

Data will be corrected for detector inefficiencies and geometry distortions

→ system specific; similar to a PET normalization

microCT uses non-iterative methods similar to a FBP used in PET reconstruction

→ cone beam recon, Feldkamp





# ComputedX-ray tomography

Bone Biology using CT

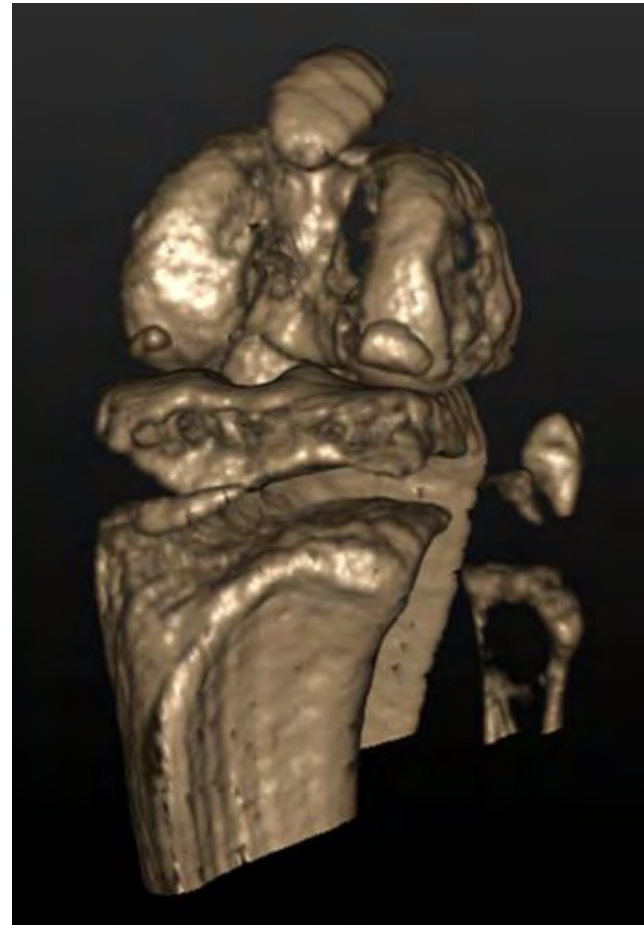


Easy to capture whole body CT

Digital zoom for high resolution CT imaging

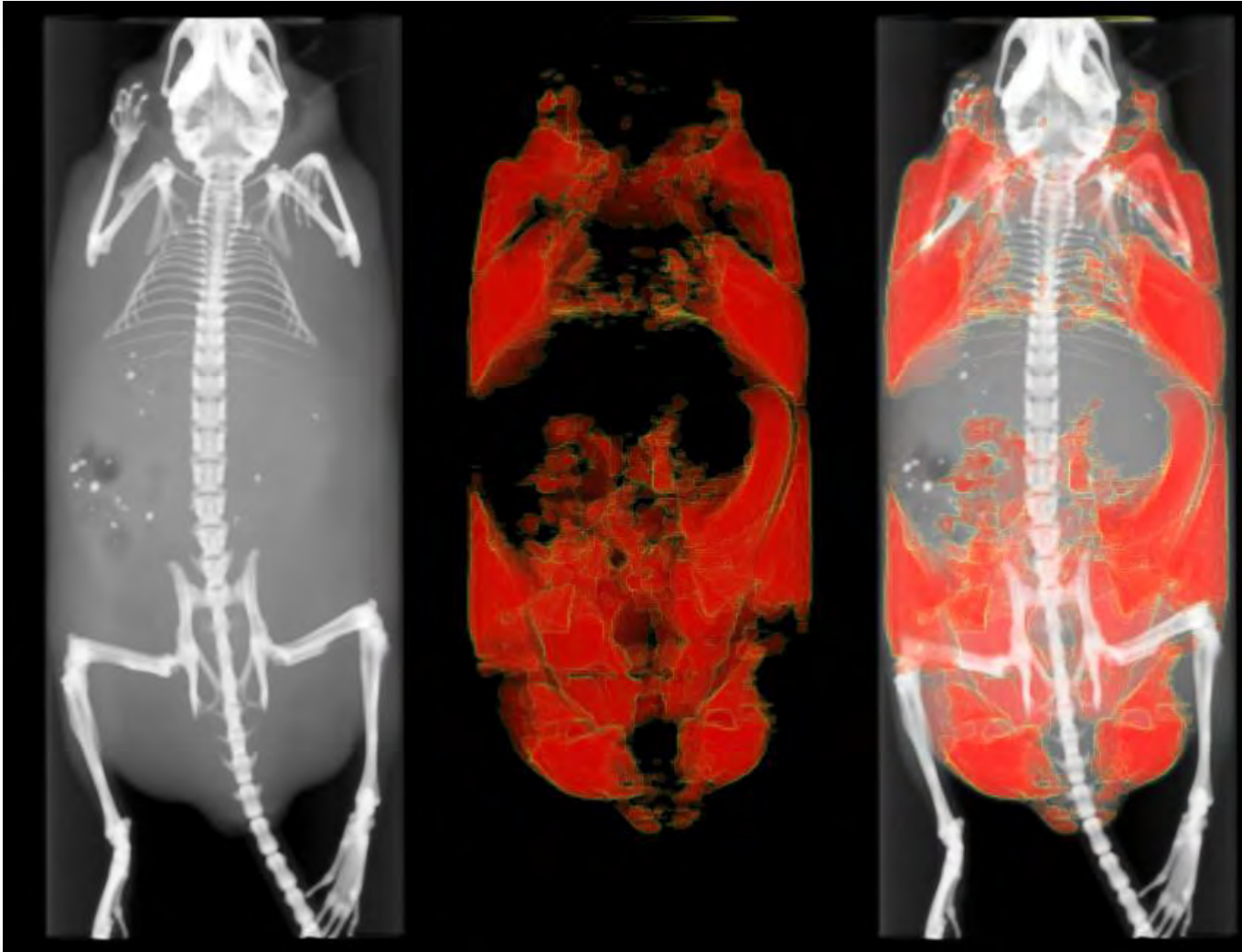
Bone size and volume quantifiable via PMOD

High resolution renderings of mouse knee achievable through  $<35 \mu\text{m}$  voxels



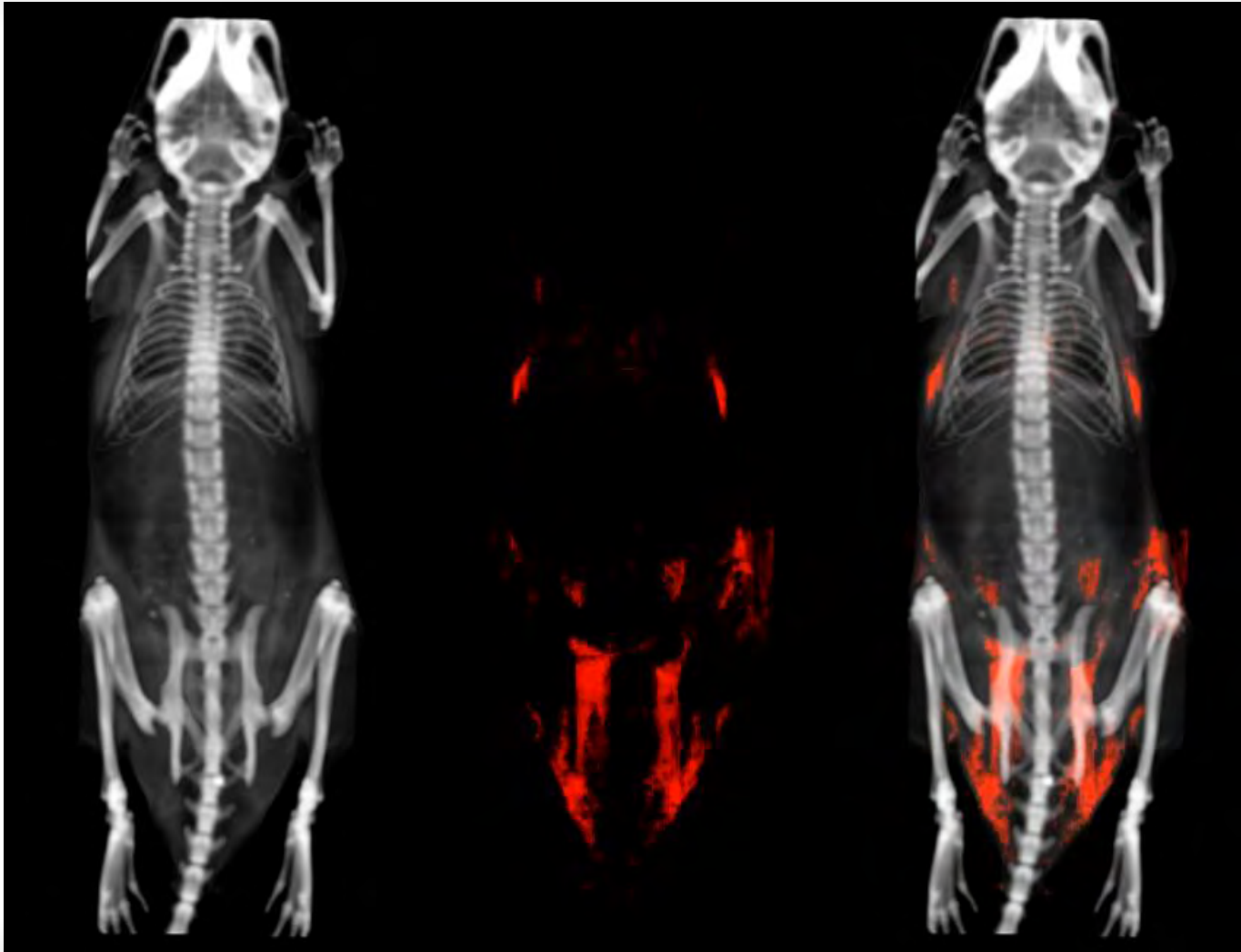
# Computed X-ray tomography

Segmentation of adipose tissue – obese mouse



# Computed X-ray tomography

Segmentation of adipose tissue – normal mouse



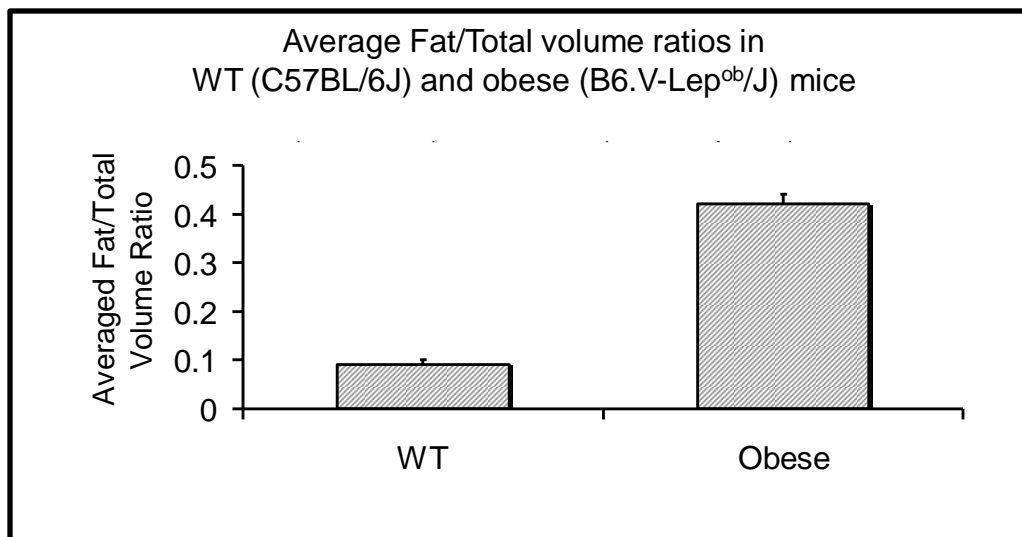
# Computed X-ray tomography

## Analysis of segmented fat areas

### WT (C57BL/6J)

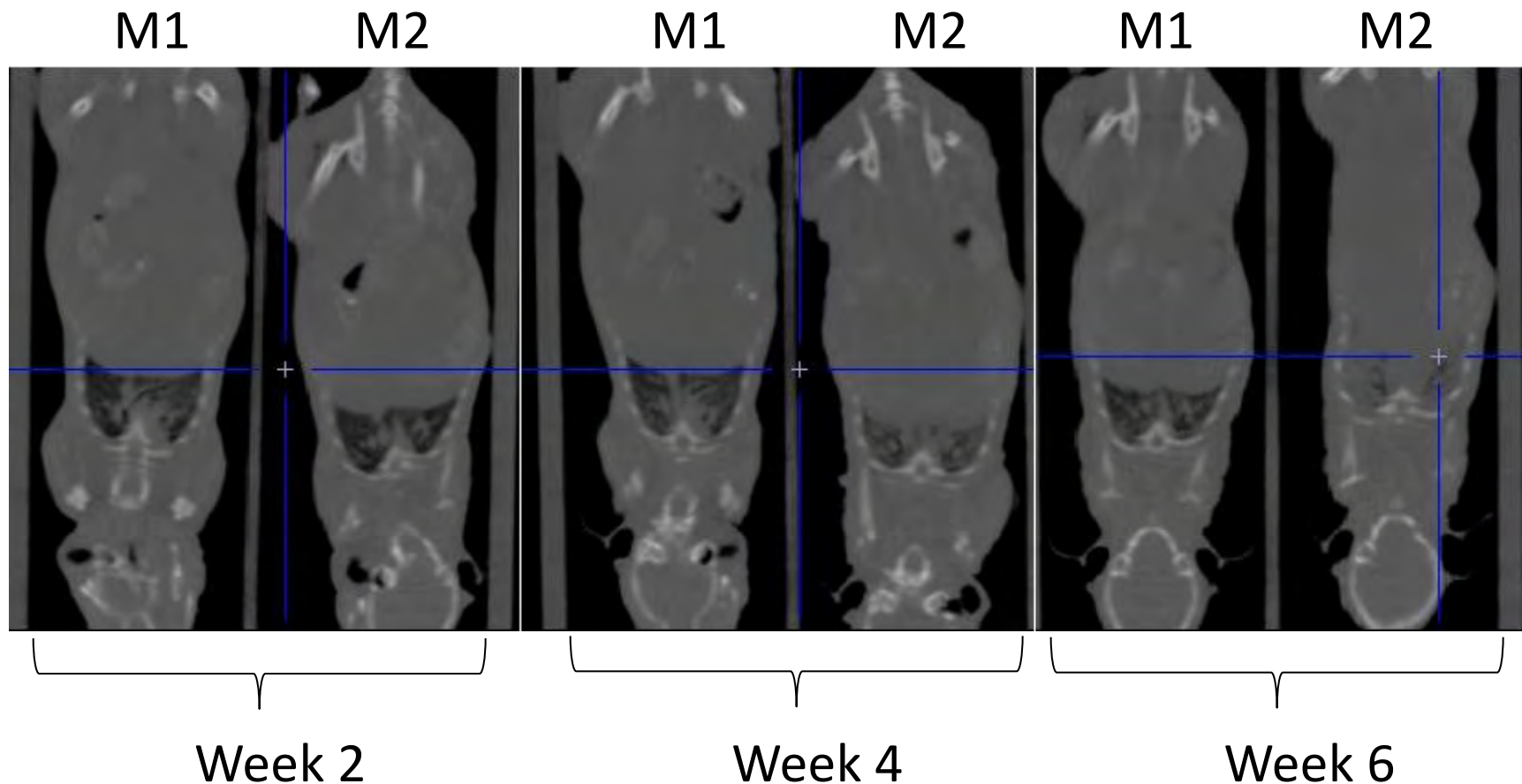
### Obese (B6.V-Lep<sup>ob</sup>/J)

|          | Total (cm <sup>3</sup> ) | Fat (cm <sup>3</sup> ) | <u>Fat</u><br><u>Total</u> |          | Total (cm <sup>3</sup> ) | Fat (cm <sup>3</sup> ) | <u>Fat</u><br><u>Total</u> |
|----------|--------------------------|------------------------|----------------------------|----------|--------------------------|------------------------|----------------------------|
| Animal 1 | 28.79                    | 3.00                   | 0.10                       | Animal 1 | 66.25                    | 26.75                  | 0.40                       |
| Animal 2 | 33.25                    | 3.05                   | 0.09                       | Animal 2 | 61.15                    | 26.31                  | 0.43                       |
| Animal 3 | 30.30                    | 2.63                   | 0.09                       | Animal 3 | 64.19                    | 25.7                   | 0.40                       |
|          |                          |                        |                            | Animal 4 | 54.25                    | 23.78                  | 0.44                       |



# Computed X-ray tomography

Decrease in Lung Volume – Metastatic Mamacarcinom



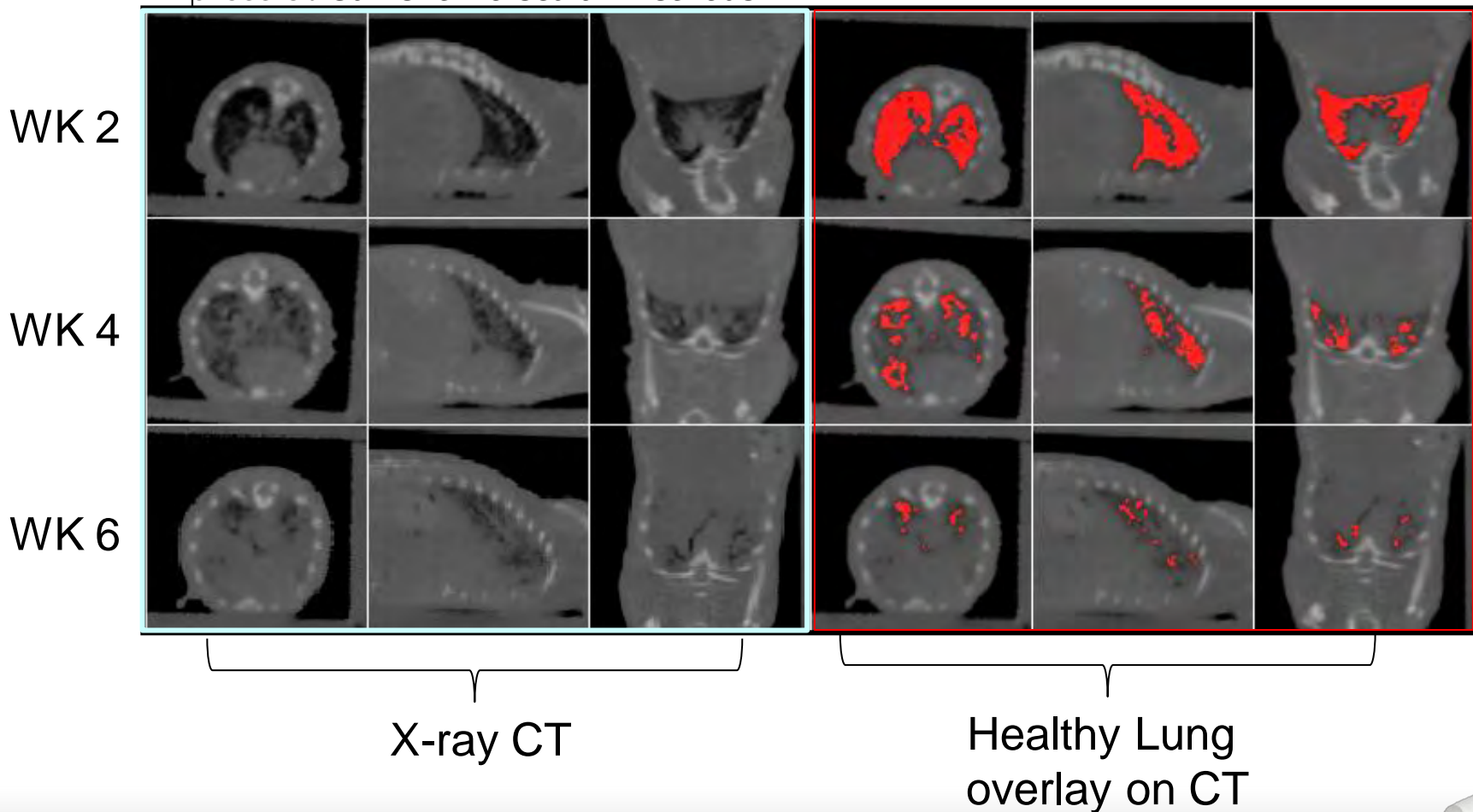
Animals imaged two at a time (Good resolution, 400 projections, 250  $\mu\text{m}$  voxel size)

# Computed X-ray tomography

Tumor mediated Lung Degradation – Longitudinal Study



In press at *Current Molecular Methods*



X-ray CT

Healthy Lung overlay on CT



# Computed X-ray tomography

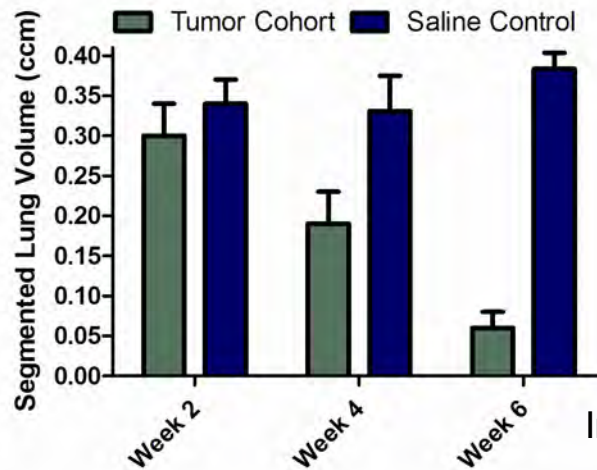
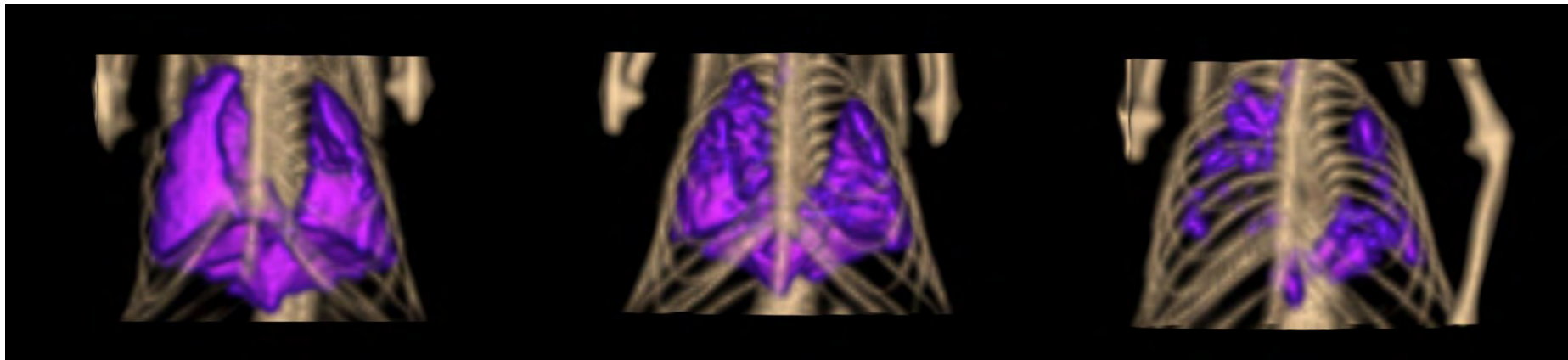
Healthy Lung Degradation – Longitudinal Study



Week 2

Week 4

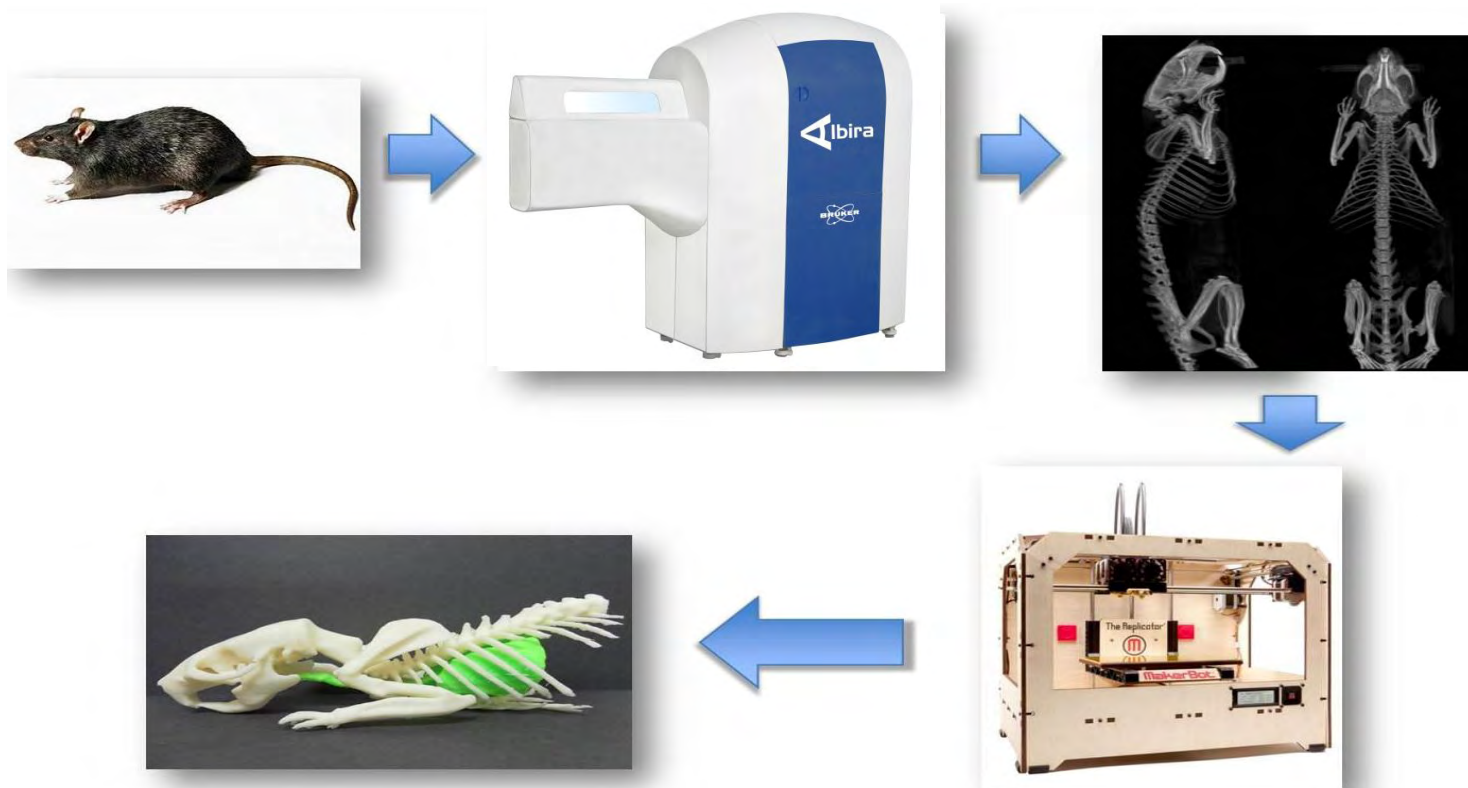
Week 6



In press at *Current Molecular Methods*

# Computed X-ray tomography

## 3D Printing of preclinical X-ray CT Data Sets





# Computed X-ray tomography

## 3D Printing of preclinical X-ray CT Data Sets



Rat Skeleton  
and Lungs



Rabbit Skull



ProJet 3000  
Overnight

Shapeways Inc.

MakerBot

# Computed X-ray tomography

## CT Contrast Agents



### Radiographic Contrast Agents:

Any substance that renders an organ or structure more visible than is possible without its addition.

Allows visualization of structures that can not be seen well or at all under normal circumstances.

### Radiographic Contrast Agents are needed because:

soft tissue has a low absorption/interaction ratio

Absorption depends on:

- atomic number

- atomic density

- electron density

- part thickness

- K-shell binding energy (K-edge)



# Computed X-ray tomography

CT Contrast Agents – Why does it work?



|               | <b>Atomic<br/>Number</b> | <b>Atomic<br/>Density</b> | <b><u>Electrons</u><br/>cm<sup>3</sup></b> | <b>Main<br/>Element</b> |
|---------------|--------------------------|---------------------------|--|-------------------------|
| <b>Air</b>    | 7.64                     | 0.00129                   | 0.0039x10 <sup>23</sup>                    | Oxygen                  |
| <b>Fat</b>    | 5.92                     | 0.91                      | 3.27x10 <sup>23</sup>                      |                         |
| <b>Water</b>  | 7.42                     | 1.00                      | 3.34x10 <sup>23</sup>                      | Oxygen                  |
| <b>Bone</b>   | 13.8                     | 1.85                      | 5.5x10 <sup>23</sup>                       | Calcium                 |
| <b>Iodine</b> | 53                       | 4.93                      |  | Iodine                  |
| <b>Barium</b> | 56                       | 3.5                       |  | Barium                  |

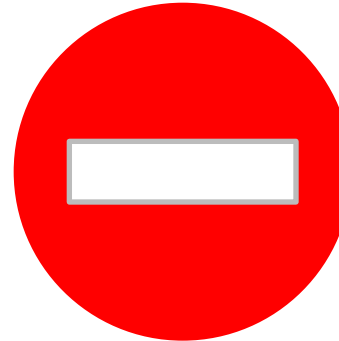


# Computed X-ray tomography

## CT Contrast Agents – Types of Contrast Media

### NEGATIVE

Air  
Oxygen  
Carbon Dioxide  
Nitrous Oxide



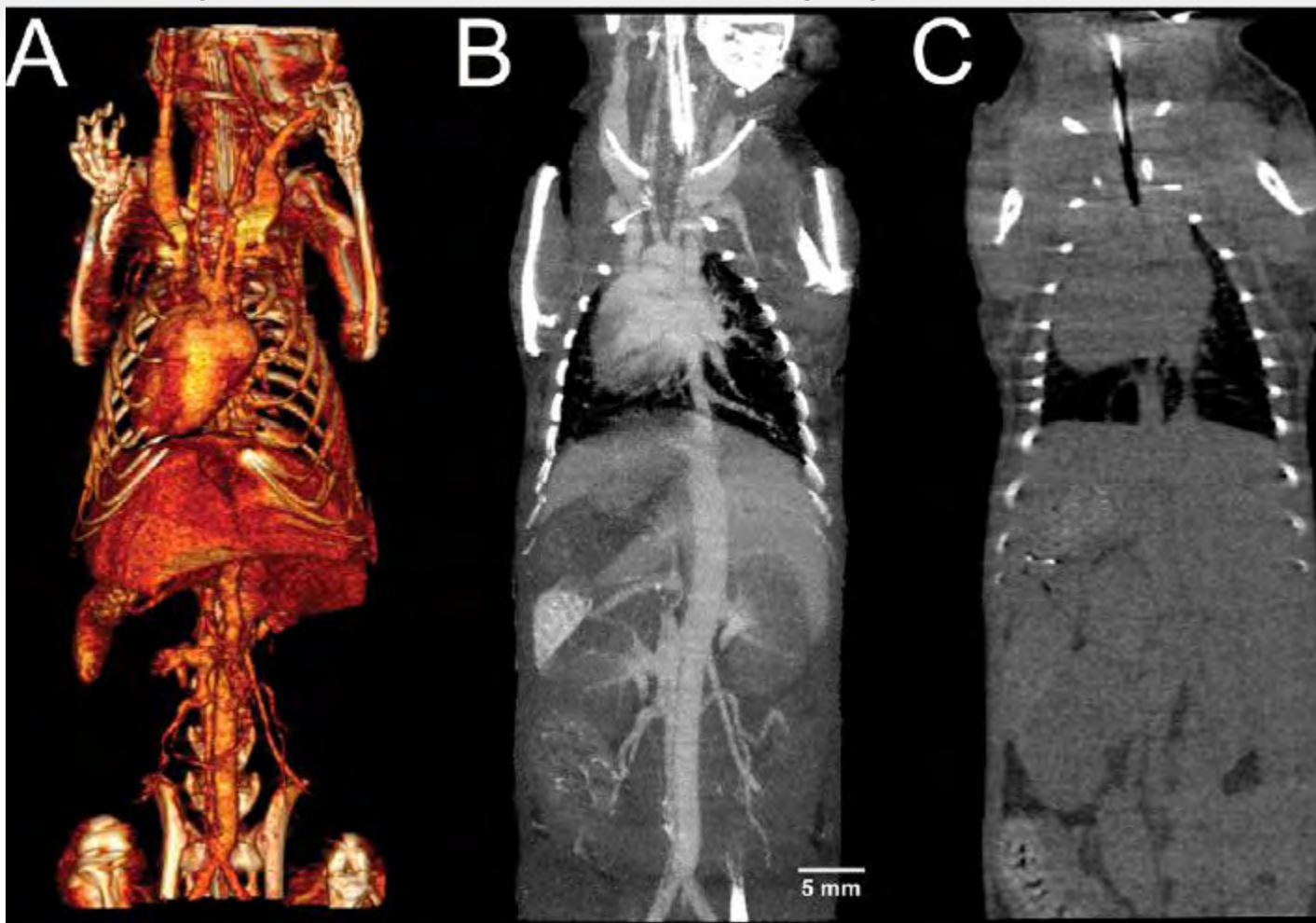
### POSITIVE

Barium  
Iodine



# Computed X-ray tomography

Contrast Agent enhanced picture – Angiography, Liver & Spleen

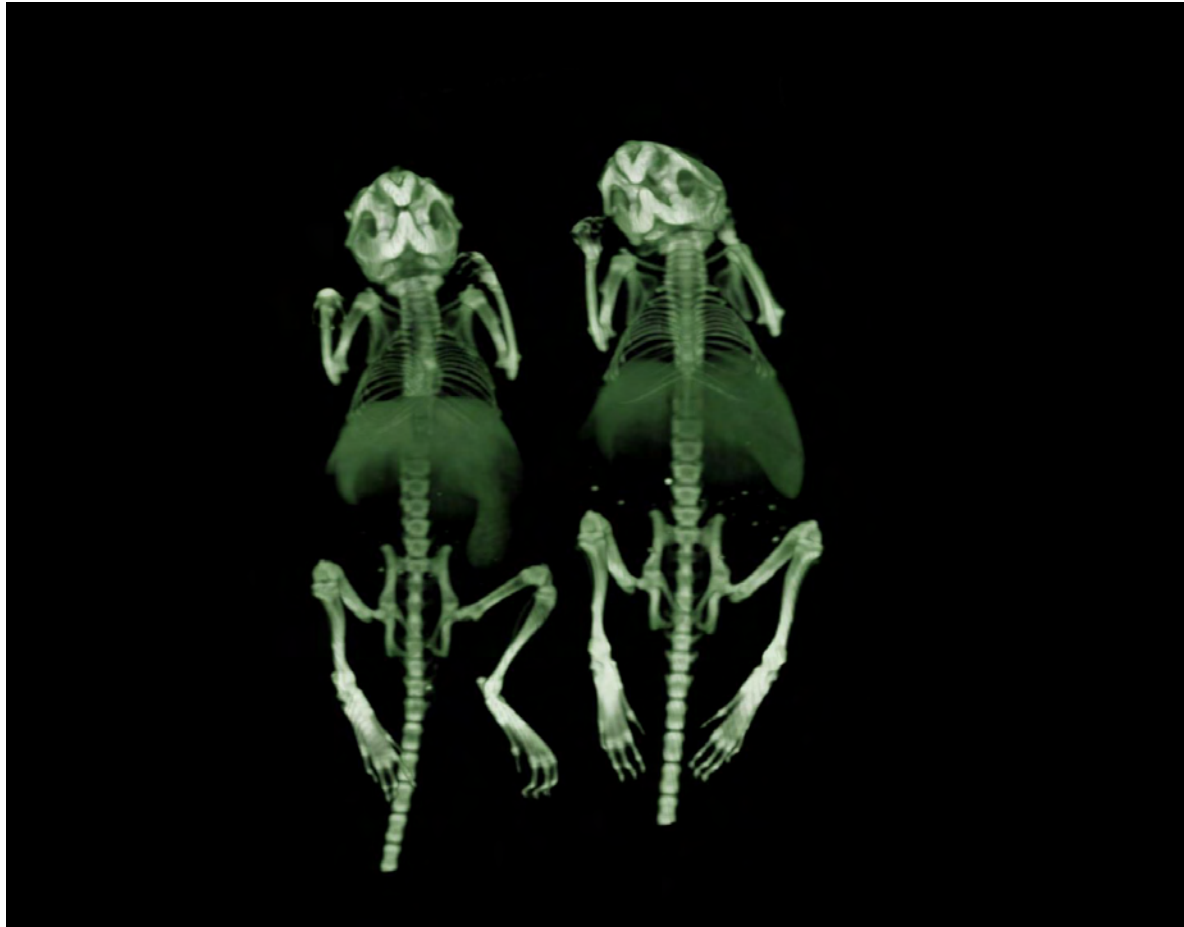


Boll H, Nittka S, Doyon F, Neumaier M, Marx A, et al. (2011) Micro-CT Based Experimental Liver Imaging Using a Nanoparticulate Contrast Agent: A Longitudinal Study in Mice PLoS ONE 6(9)



# Computed X-ray tomography

Novel Liver Contrast Agent for CT



# Computed X-ray tomography

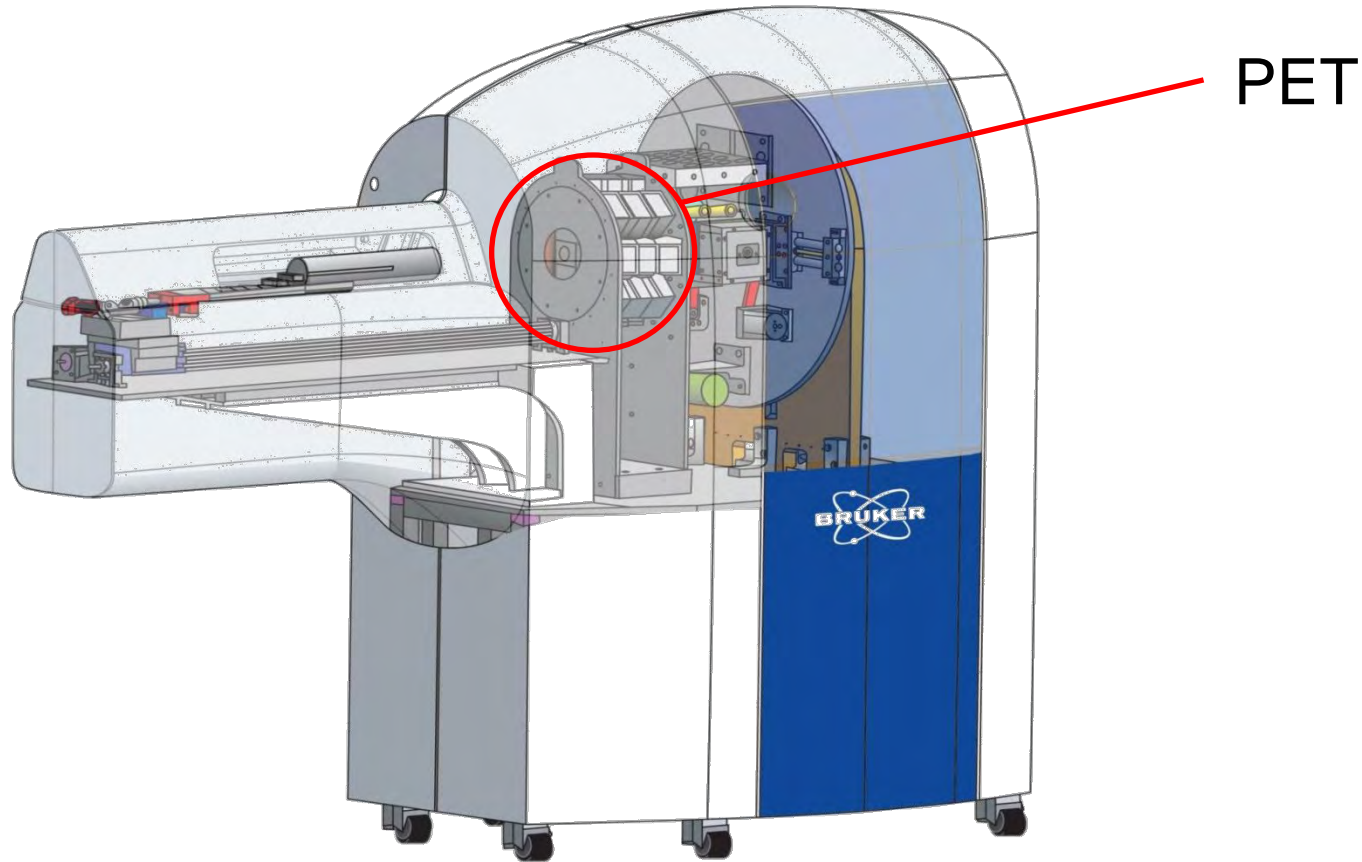
Novel Contrast Agent for CT of Vascular System



Contrast Media = Aurovist

# Positron Emission Tomography

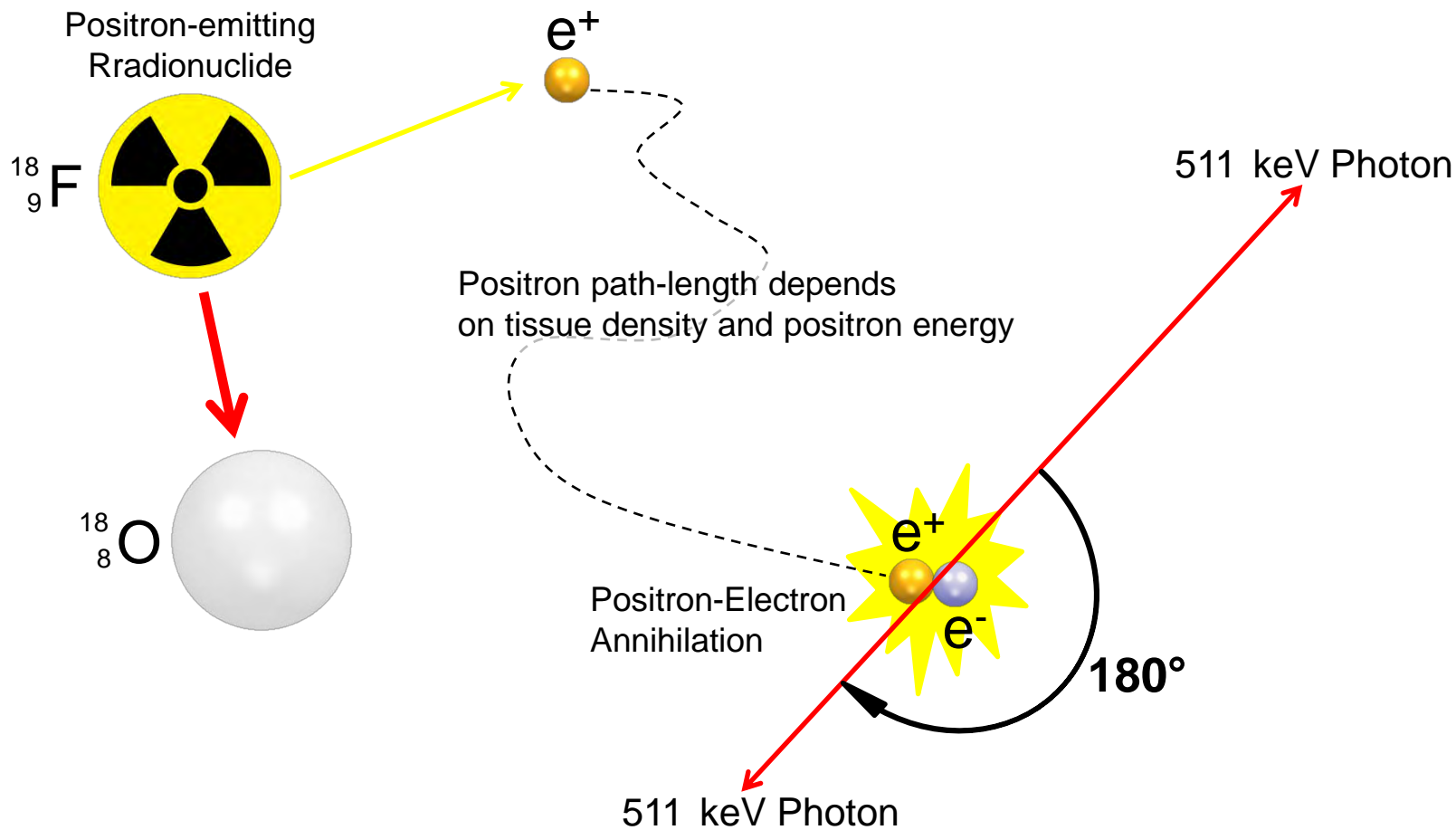
## PET





# Positron Emission Tomography

## Positron – Electron Annihilation



# Positron Emission Tomography

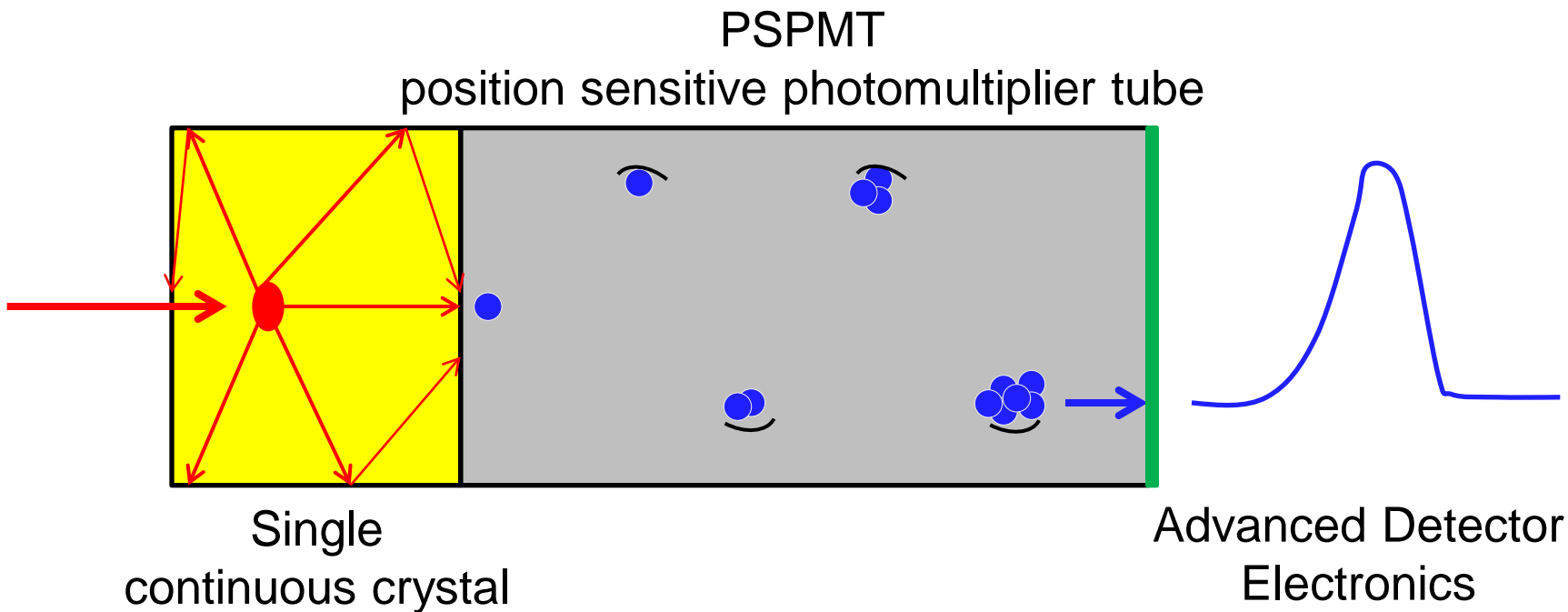
## Positron Emitting Radionuclides

| Isotope | Halflife   | $\beta^+$ fraction | Max. Energy | range(mm) |
|---------|------------|--------------------|-------------|-----------|
| C-11    | 20.4 mins  | 0.99               | 0.96 MeV    | 0.4 mm    |
| N-13    | 9.96 mins  | 1.00               | 1.20 MeV    | 0.7 mm    |
| O-15    | 123 secs   | 1.00               | 1.74 MeV    | 1.1 mm    |
| F-18    | 110 mins   | 0.97               | 0.63 MeV    | 0.3 mm    |
| Cu-62   | 9.74 mins  | 0.98               | 2.93 MeV    | 2.7 mm    |
| Cu-64   | 12.7 hours | 0.19               | 0.65 MeV    | 0.3 mm    |
| Ga-68   | 68.3 mins  | 0.88               | 1.83 MeV    | 1.2 mm    |
| Br-76   | 16.1 hours | 1.00               | 1.90 MeV    | 1.2 mm    |
| Rb-82   | 78 secs    | 0.96               | 3.15 MeV    | 2.8 mm    |
| I-124   | 4.18 days  | 0.22               | 1.50 MeV    | 0.9 mm    |



# Positron Emission Tomography

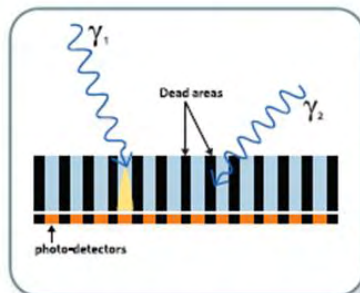
ALBIRA Gamma-ray Detector Principle



# Positron Emission Tomography

## Positron – Electron Annihilation

### Conventional Technology

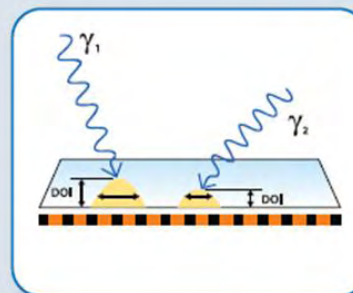


Pixelated crystal technology with dead zones.

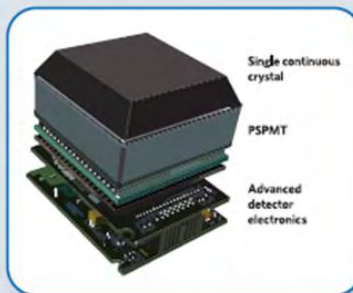


Standard PET detector technology

### Albira Technology



Simultaneous detection of position and DOI measurement. No dead zones.

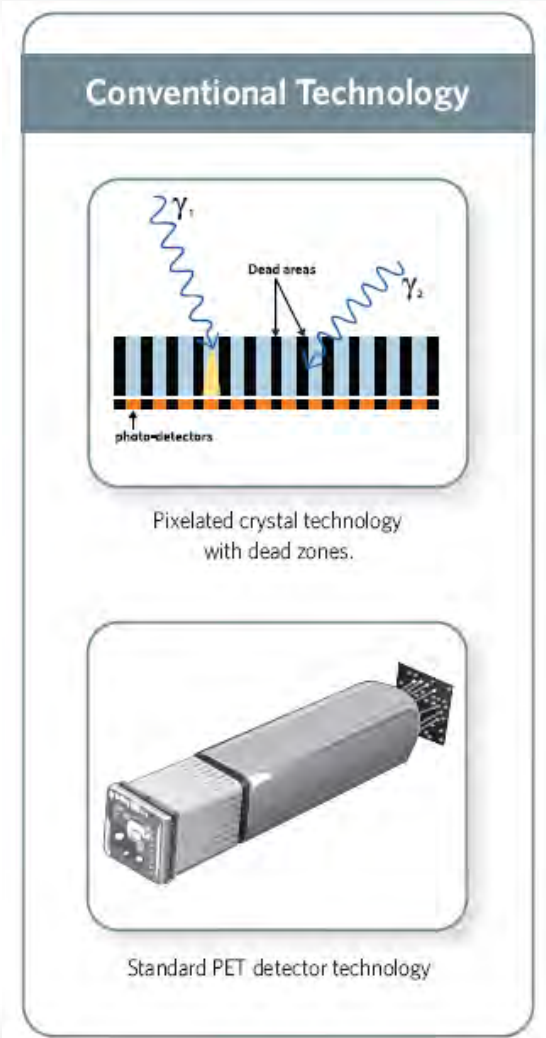


Albira's exclusive patented PET detector



# Positron Emission Tomography

## Positron – Electron Annihilation



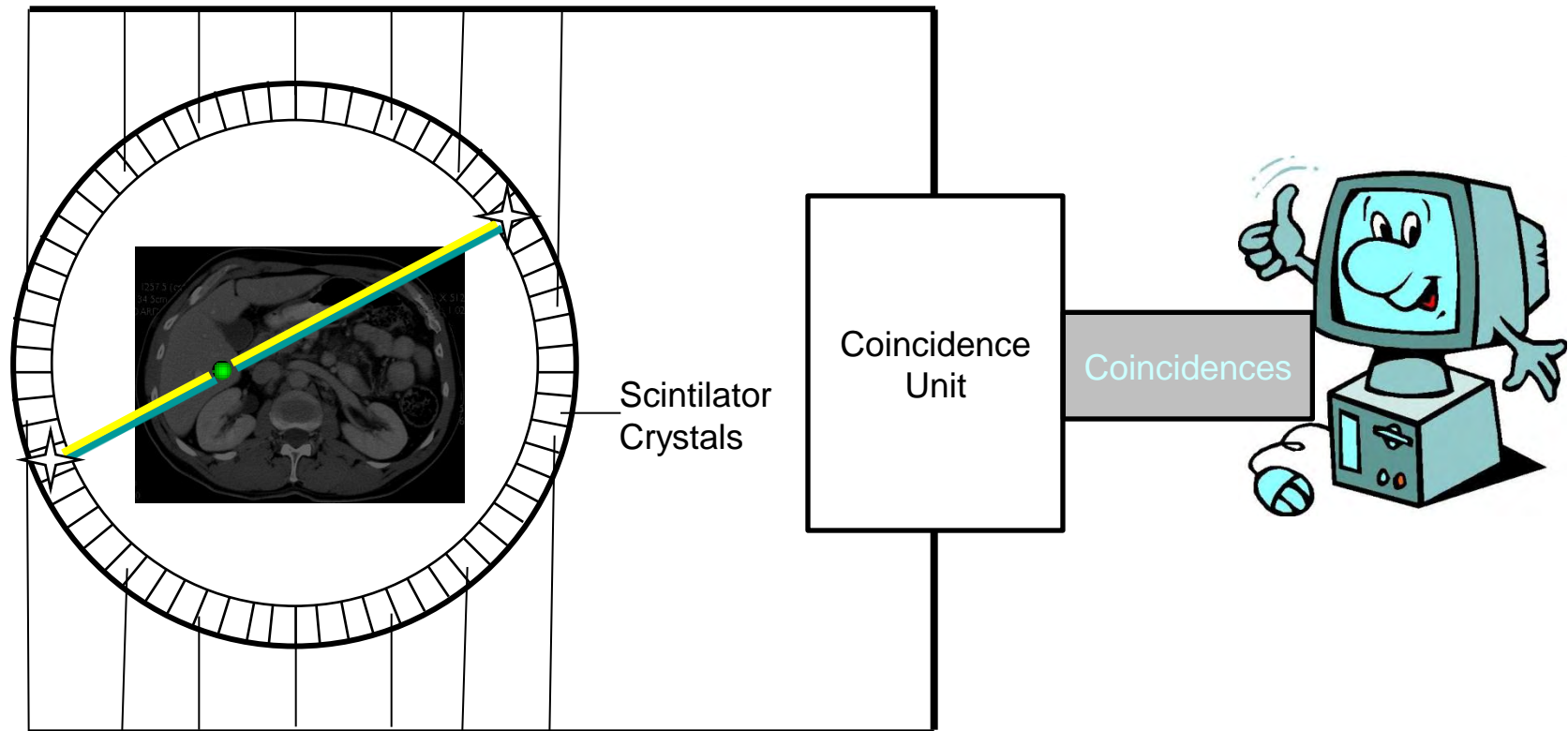
Current technology utilized packed crystals with dead zones

Tighter packing yields more dead zones

Susceptible to the parallax error

# Positron Emission Tomography

Operation of a PET-Scanner



# Positron Emission Tomography

$\gamma$ -ray Detection in a PET system



## True Coincidences

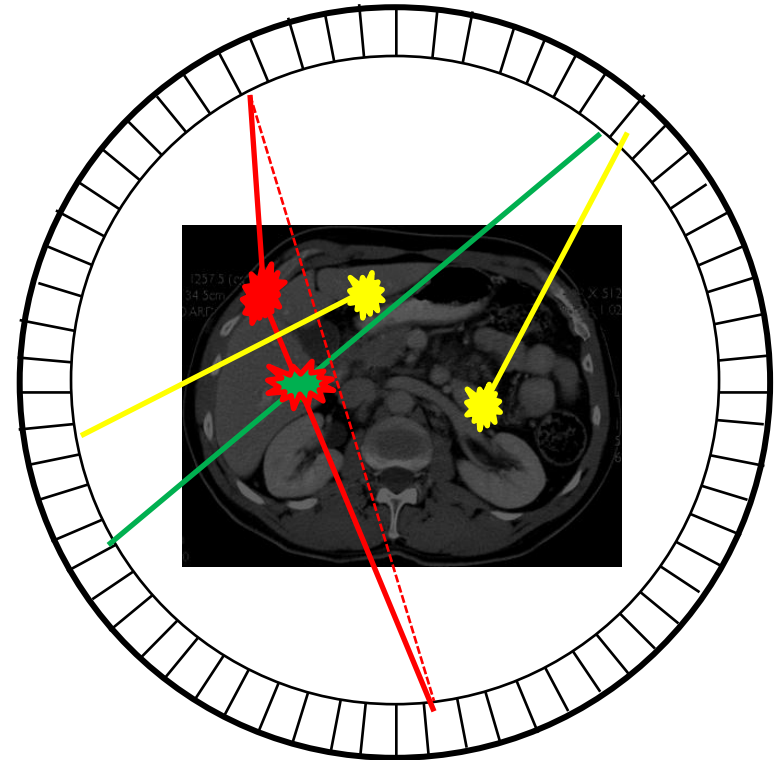
both  $\gamma$ -rays escape without scatter and interact in detectors

## Scatter coincidences

one, or both  $\gamma$ -rays scatter in tissue

## Random coincidences

two  $\gamma$ -rays from different origins strike the detectors at the same time  
(a.k.a. *accidental coincidences*)



# Positron Emission Tomography

## PET Hardware



### Scintillators

- High stopping power
- High light output
- Fast scintillator
- Small crystal size
- High spatial resolution

**LSO, LYSO, YAP, etc.**

### Light-Detectors

#### **Photomultiplier Tubes (PMT)**

- Single Channel
- Multi Channel

#### **Solid State Detectors**

- Avalanche Photo Diodes (APD)
- Geiger-Mode APDs
- Silicon-PMTs

### Detector type

- Single Crystal Coupling
- Block Detector
- Detectors with DOI capabilities (Phoswitch)

- A full PET system comprises several detector rings summing up to several 1000 to 10.000 individual crystals
- The performance of a PET system as well as physical limitations will be determined by the choice of hardware





# Positron Emission Tomography

## Important Scanner Parameters



### Energy Resolution

detection limit for measured energy of detected  $\gamma$ -rays

### Timing Resolution

time variation (inaccuracy) of the system for detection of two single events originating from the same annihilation

### Spatial Resolution

smallest object that can be visualized (partial volume effect)

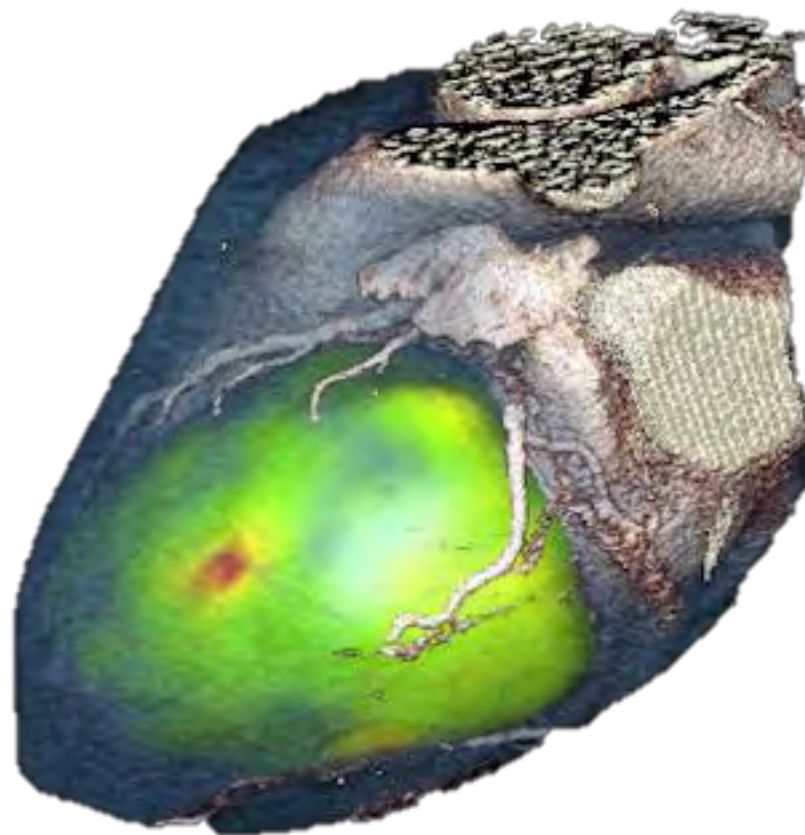
### Sensitivity

detection limit for radiotracer (isotope) or contrast media



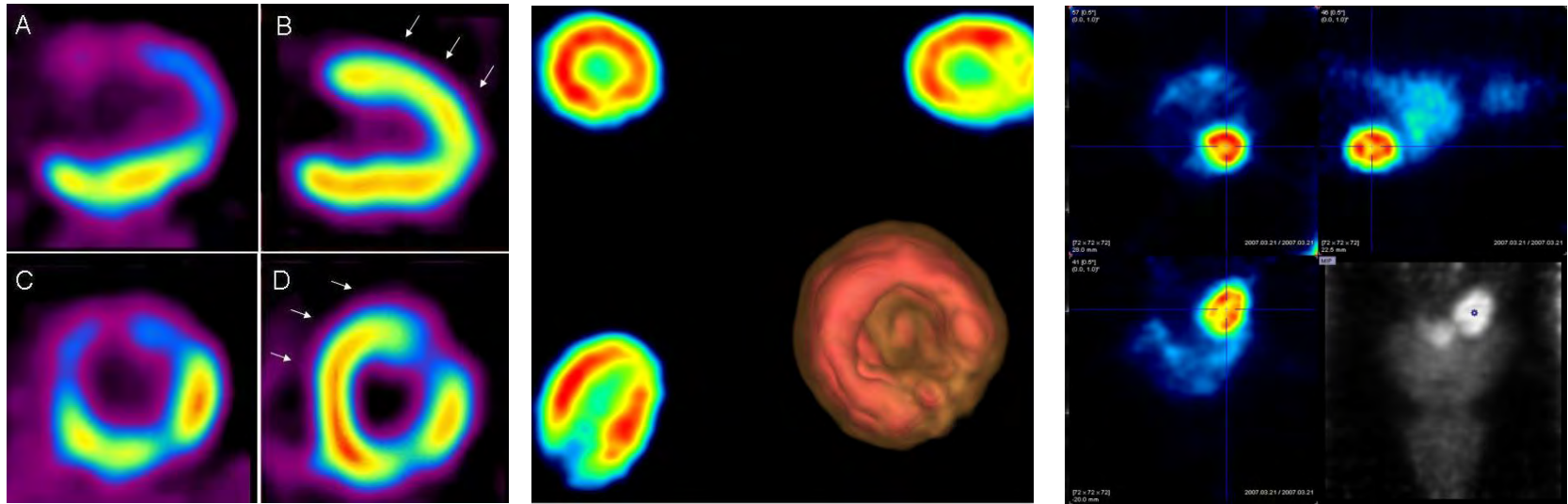
# Positron Emission Tomography

## Cardiology



# Positron Emission Tomography

Cardiology – From mouse to man



$^{18}\text{F}$ -FDG – human heart <sup>A</sup>

$^{18}\text{F}$ -FDG –rat heart <sup>B</sup>

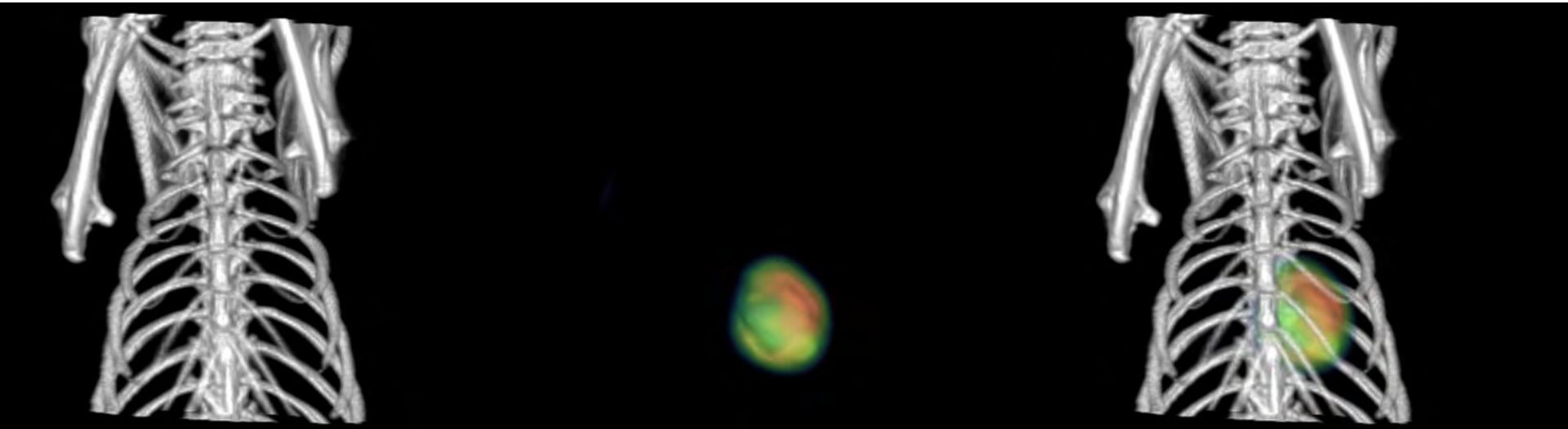
$^{18}\text{F}$ -FDG – mouse heart

<sup>A</sup> Tossios, P., et al. No evidence of myocardial restoration following transplantation of mononuclear bone marrow cells in coronary bypass grafting surgery patients based upon cardiac SPECT and  $^{18}\text{F}$ -PET. BMC Medical Imaging. (2006),

<sup>B</sup> Courtesy of Prof. J. Viña, Research Unit, Physiology Faculty, Uni. Valencia.

# Positron Emission Tomography

Cardiology - 3D imaging of a rat heart (PET/CT-Fusion)

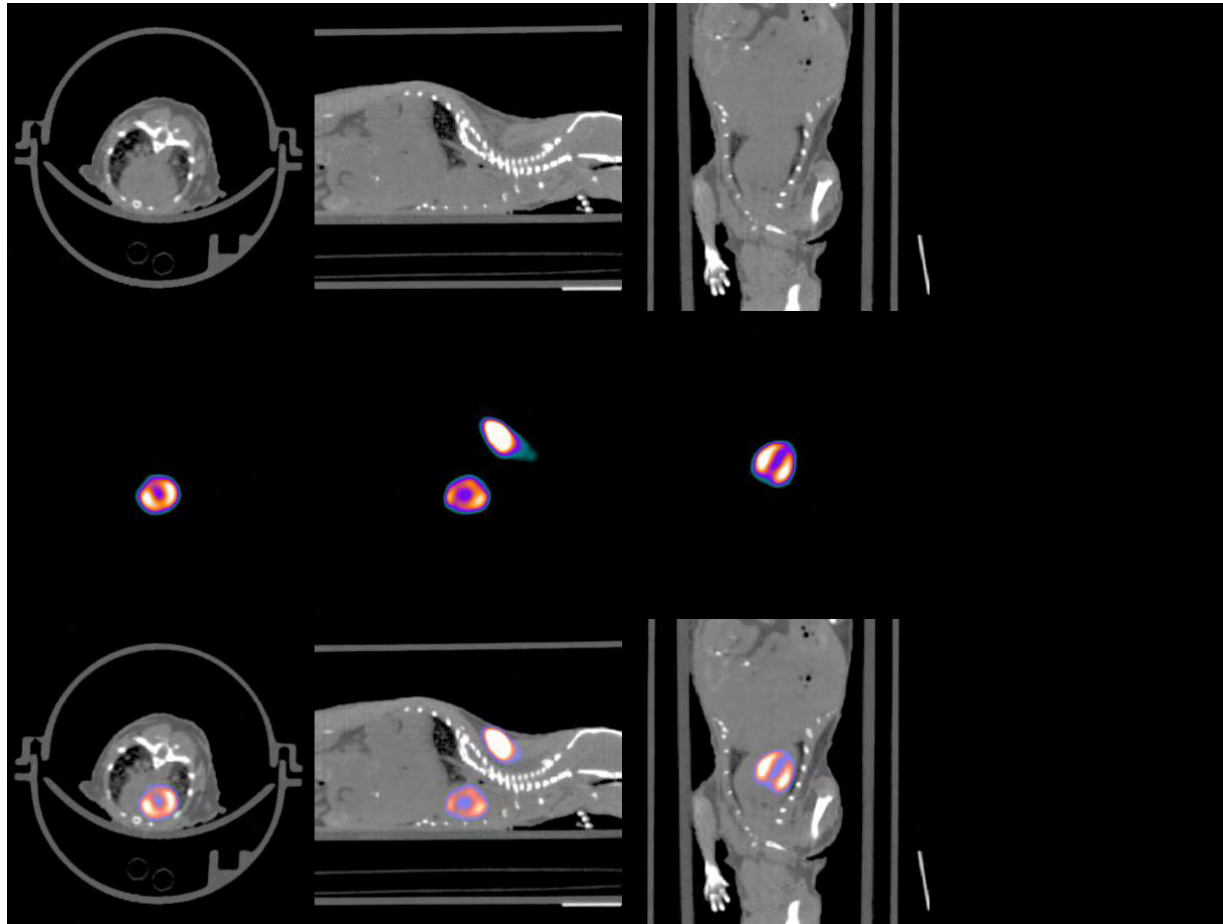


$^{18}\text{F}$ -FDG imaging of a rat heart without gating

Major walls of the heart are clearly visible

# Positron Emission Tomography

Cardiology - Mouse heart imaging - without gating



# Positron Emission Tomography

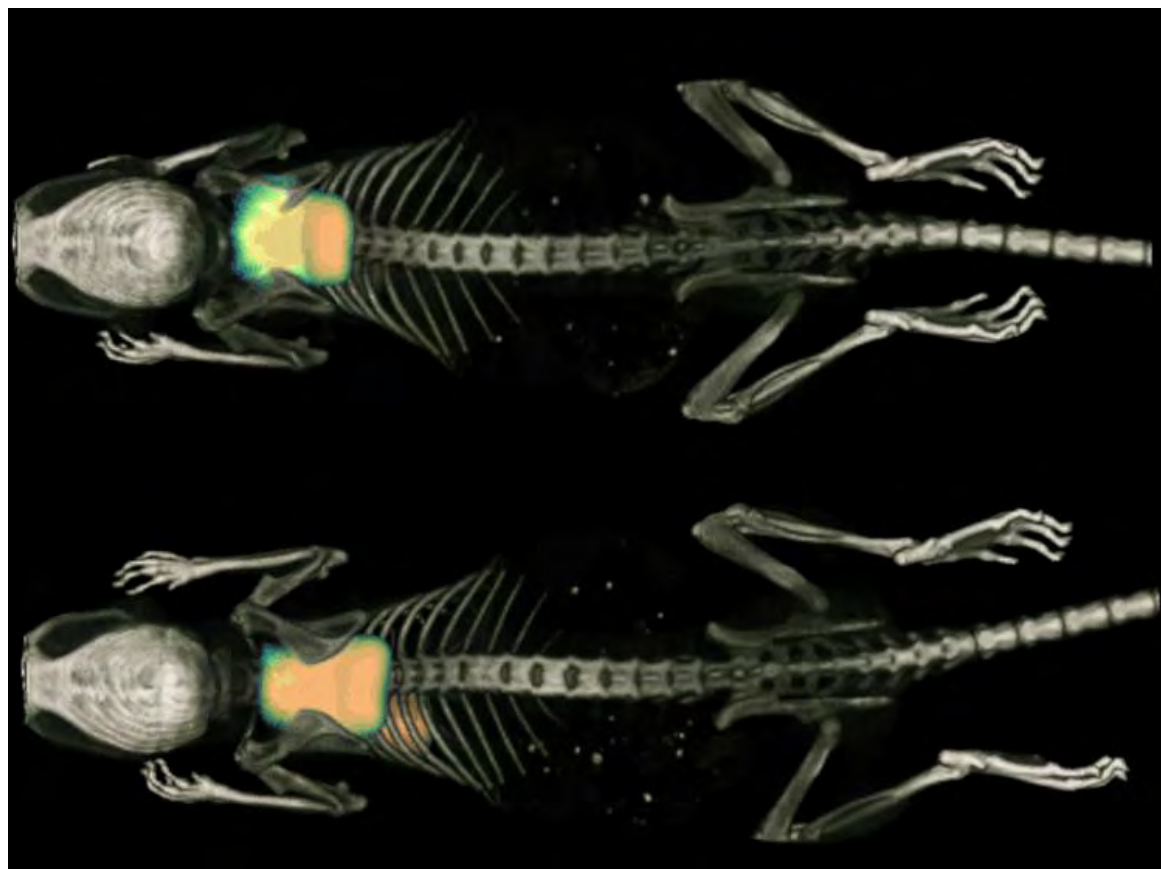
Cardiology - Mouse heart imaging - without gating



- With a high resolution PET scanner gating may not always be necessary
- Saves time and dose
- Protocol
  - 500 uCi of  $^{18}\text{F}$ -FDG injected
  - Data acquired for 10 min
  - Data reconstructed with MLEM
  - Data fused with CT

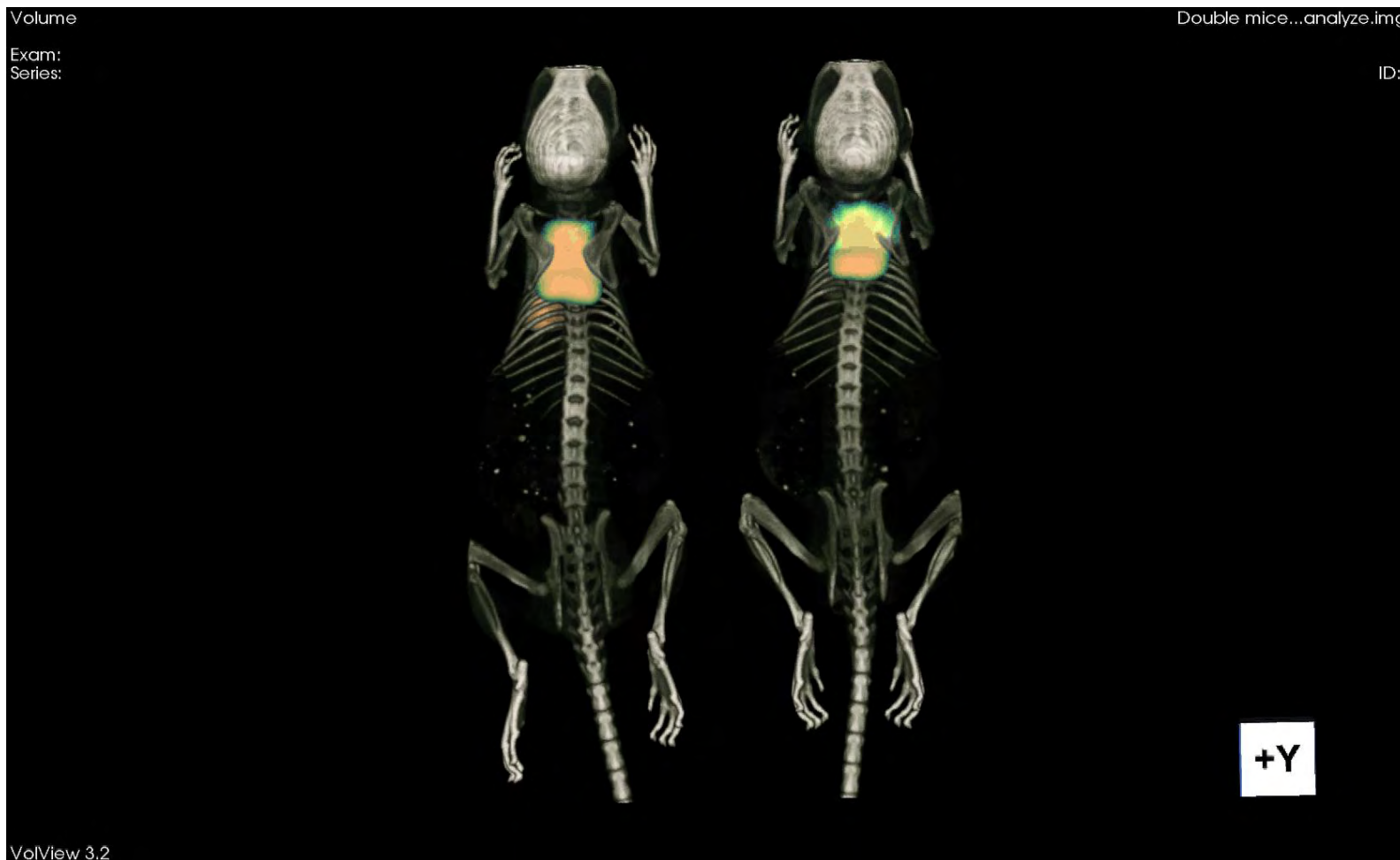
# Positron Emission Tomography

Metabolic Diseases



# Positron Emission Tomography

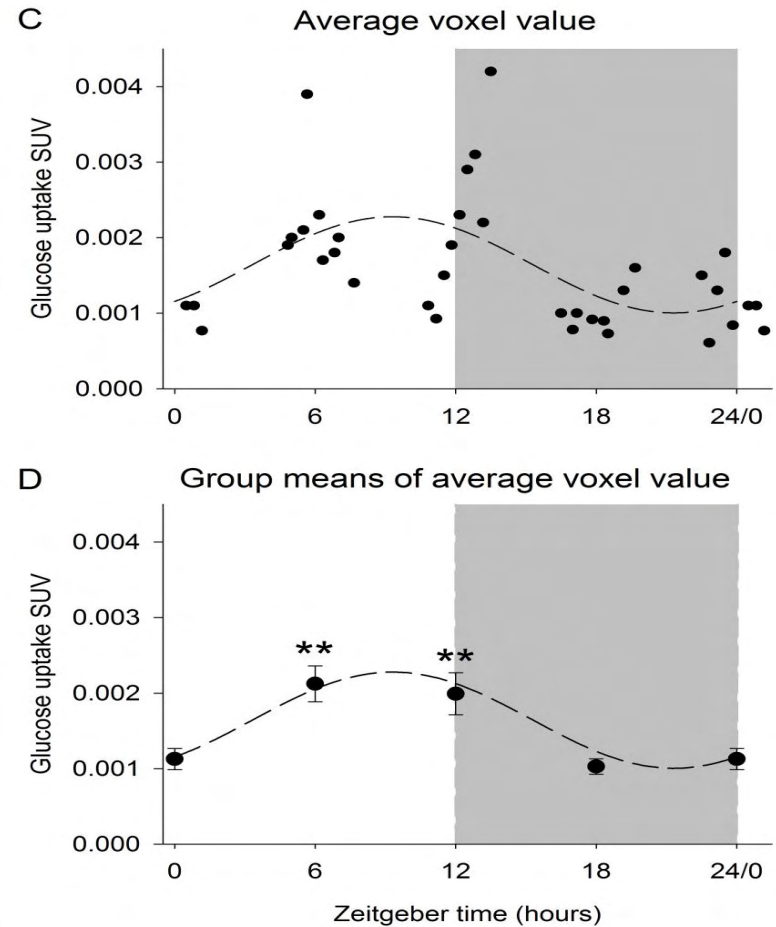
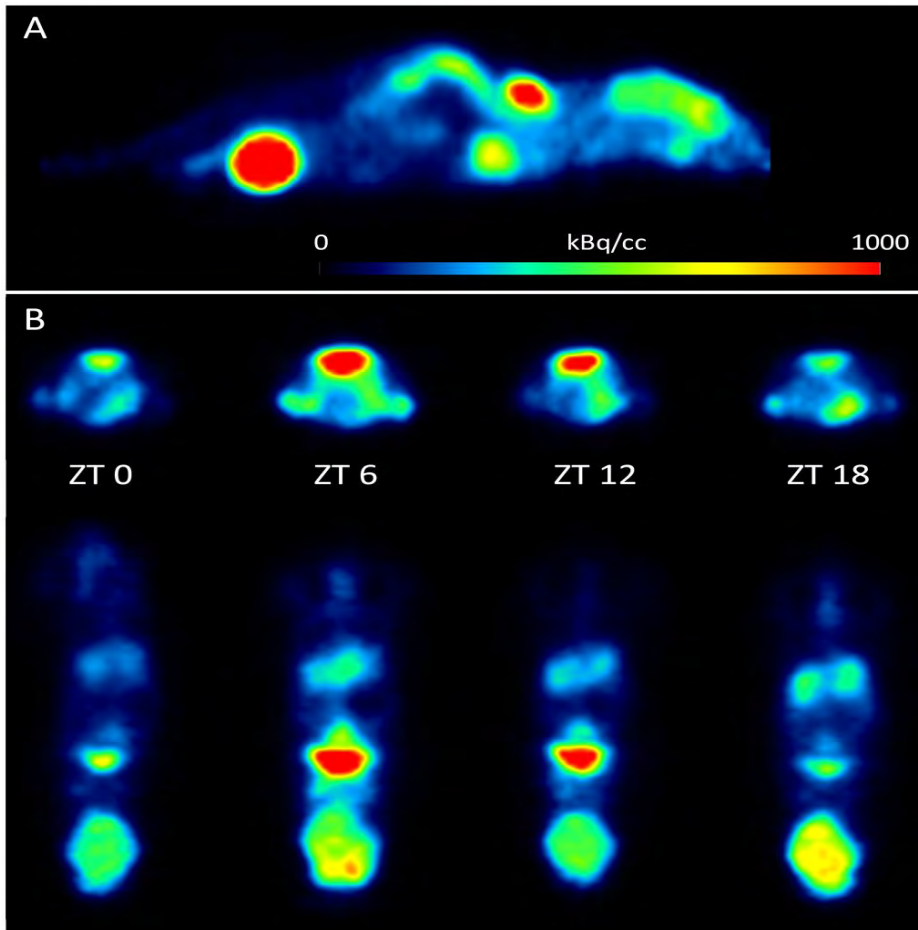
Brown fat in mice – PET/CT-fusion





# Positron Emission Tomography

Brown fat in mice – PET/CT-fusion



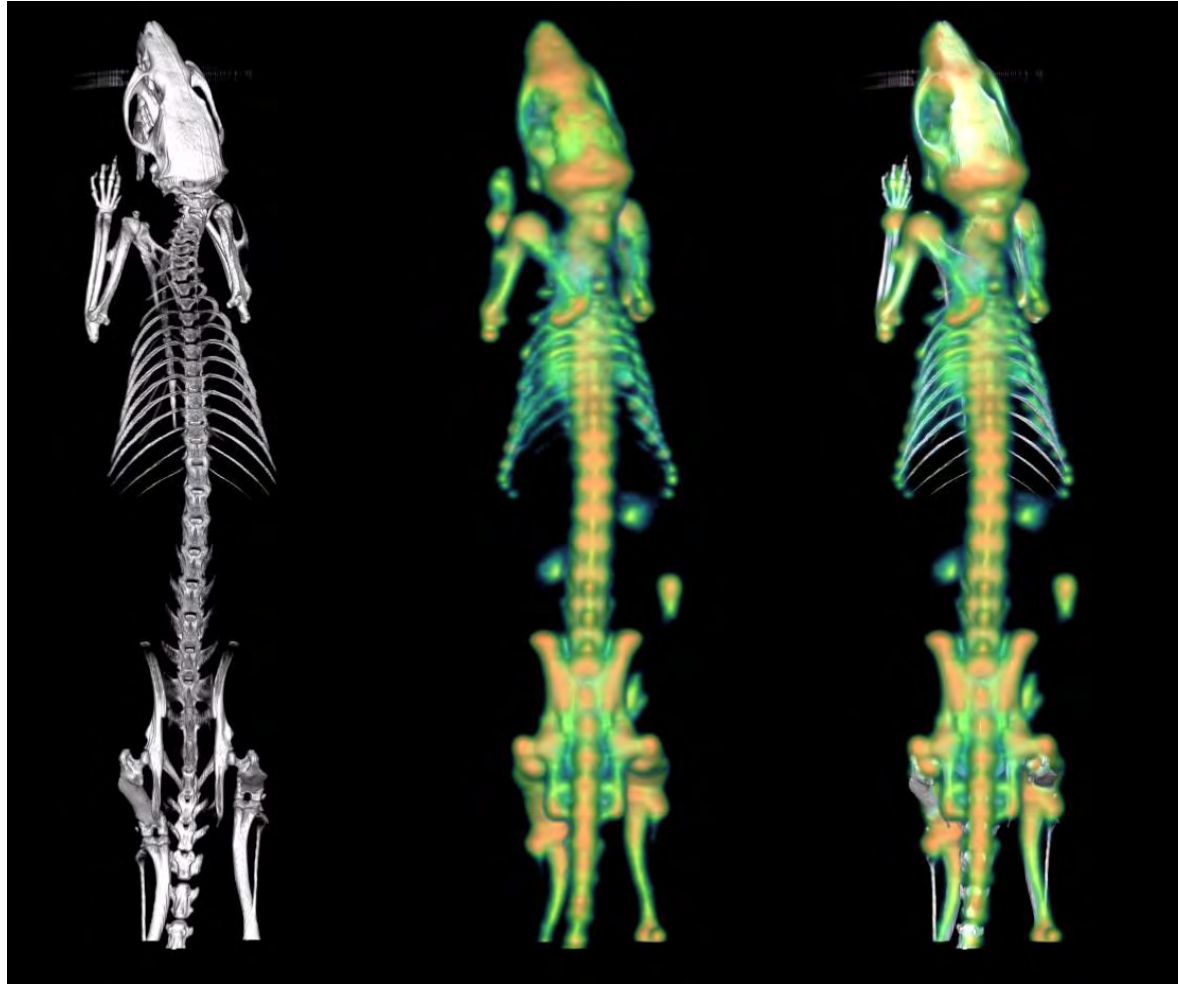
# Positron Emission Tomography

Bone Development and Bone Diseases



# Positron Emission Tomography

$^{18}\text{F}$ -NaF PET/CT imaging in rat



# Positron Emission Tomography

Bone Development in mouse – single PET scan

- Injected 200  $\mu\text{Ci}$  of  $^{18}\text{F}$  NaF
- Imaged on Albira 2 ring PET/CT
- Areas of new bone growth show significant uptake



# Positron Emission Tomography

Triple Tracer Imaging – PET/SPECT/Optical



PET/CT  
(Na<sup>18</sup>F)

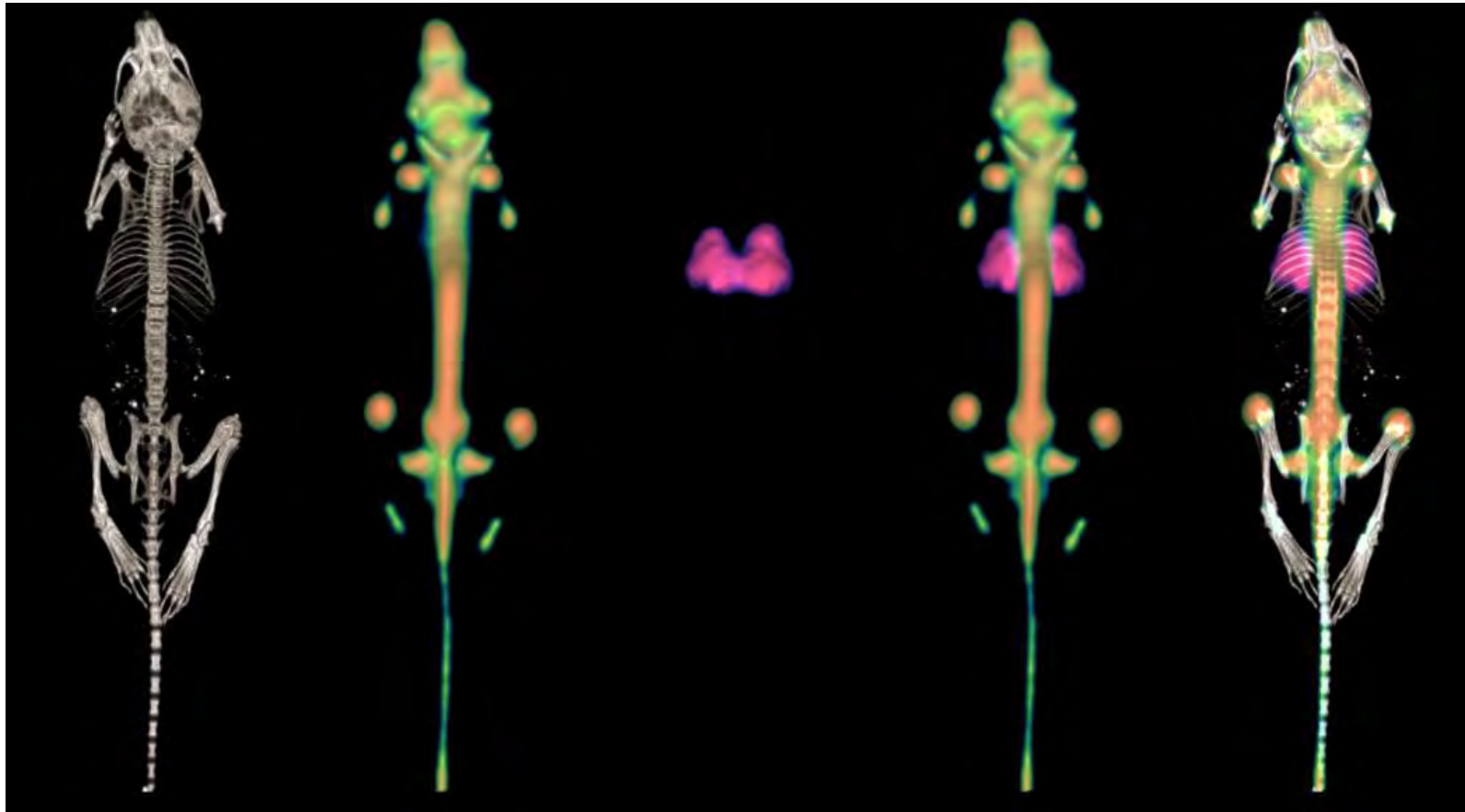
SPECT/CT  
(<sup>99m</sup>Tc-MDP)

Fluorescence/X-ray  
(Osteosense-750)



# Positron Emission Tomography

Dual Tracer Mouse Scan – PET/SPECT/CT



CT

PET  
( $\text{Na}^{18}\text{F}$ )

SPECT  
( $^{99\text{m}}\text{Tc-MAA}$ )

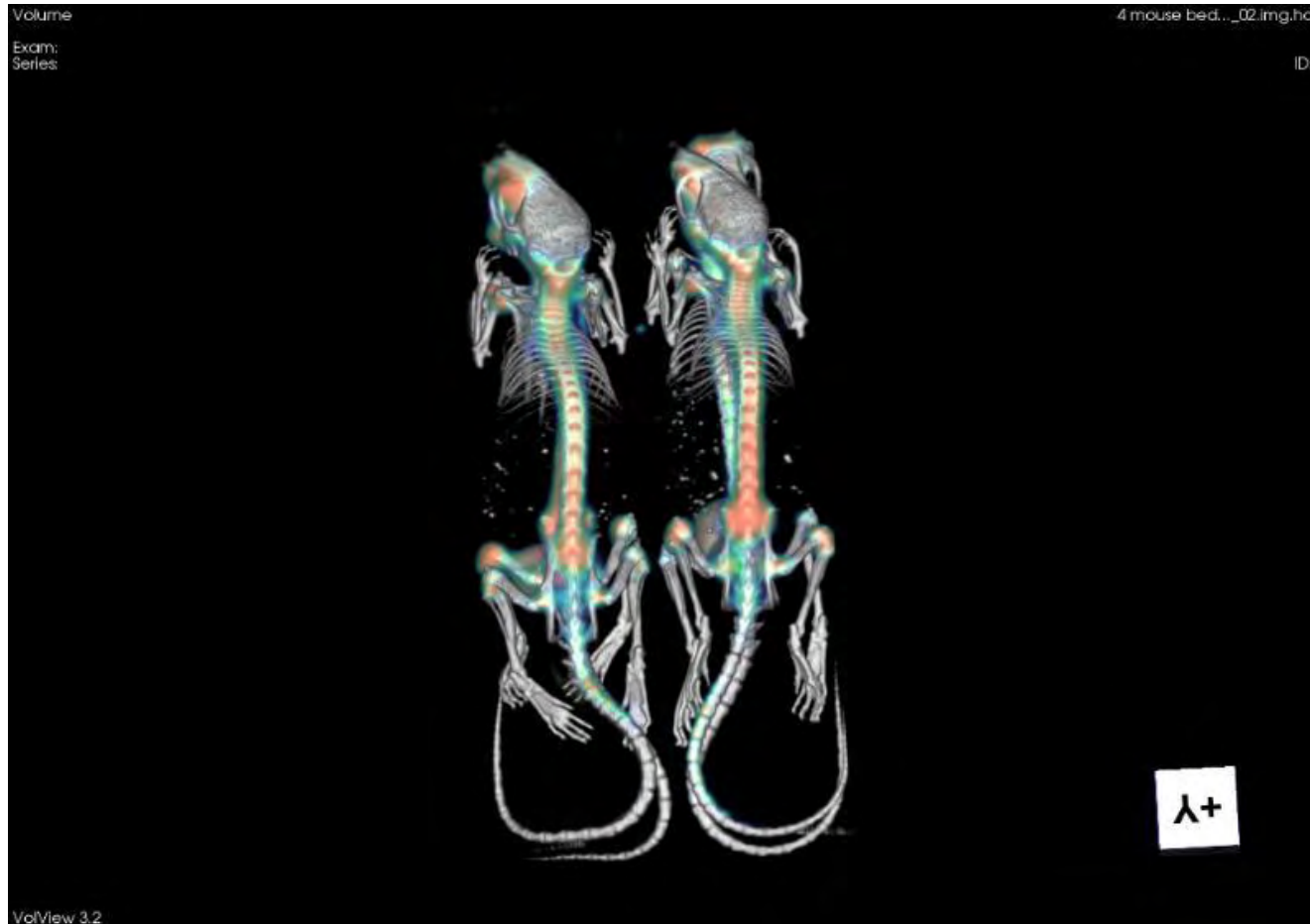
PET/SPECT  
Overlay

Trimodal Overlay



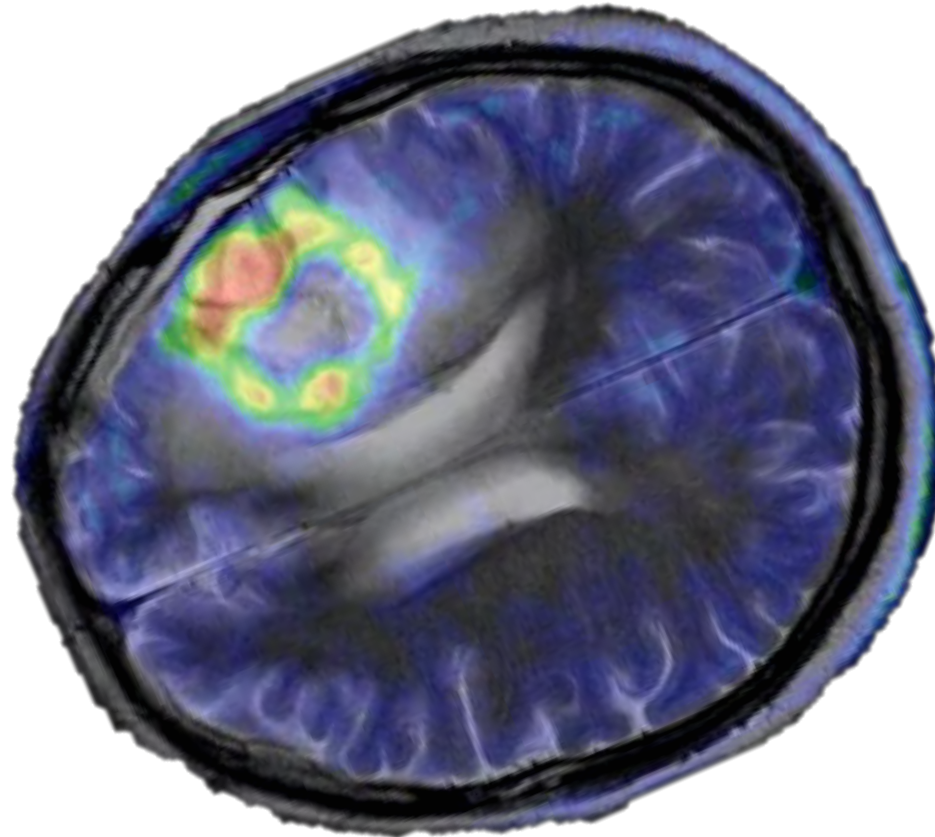
# Positron Emission Tomography

$^{18}\text{F}$ -NaF – Four Mice PET/CT



# Positron Emission Tomography

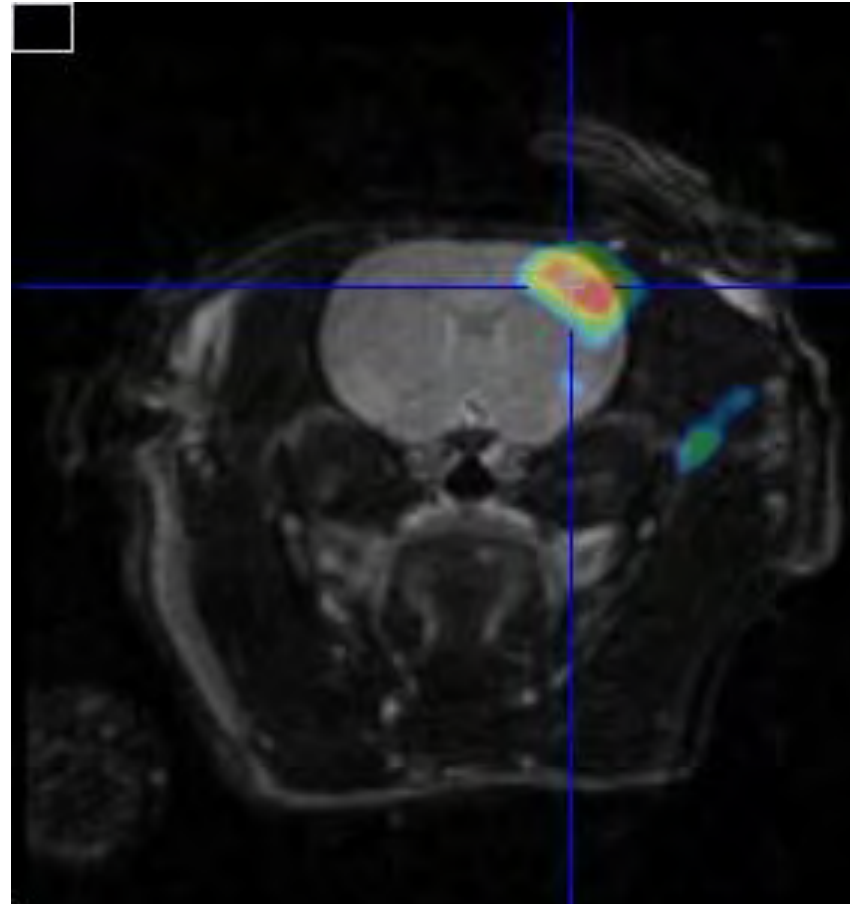
Neurology – Functional Brain imaging





# Positron Emission Tomography

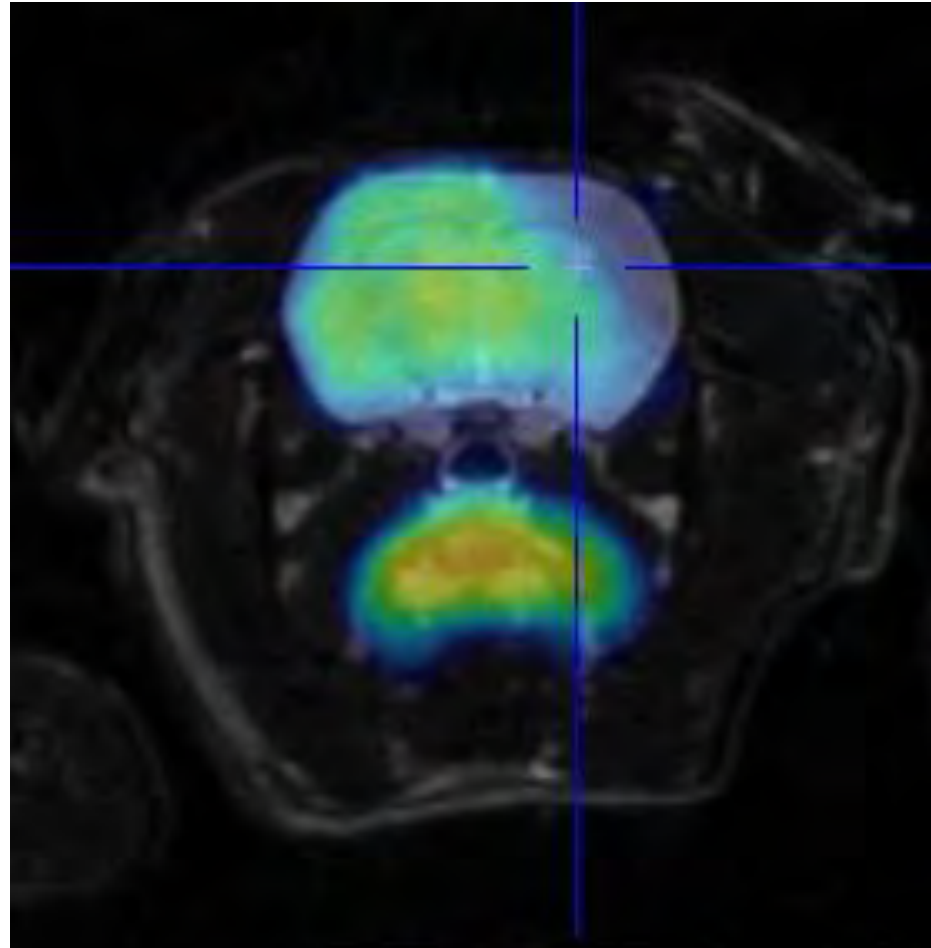
$^{18}\text{F}$ -FMISO – identification of hypoxic lesions in the brain



$^{18}\text{F}$ -FMISO in rats

# Positron Emission Tomography

$^{18}\text{F}$ -FDG Brain Metabolism after Ischemic Injury



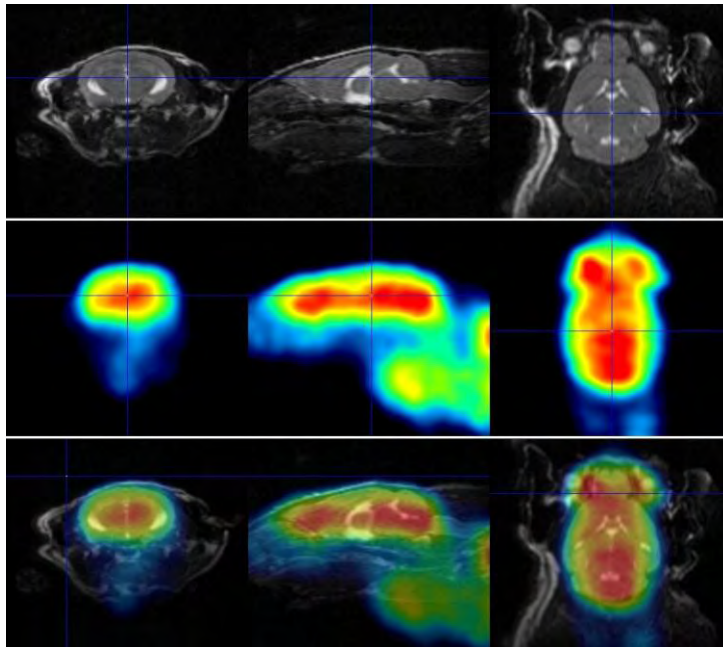
$^{18}\text{F}$ -FDG in rats

# Positron Emission Tomography

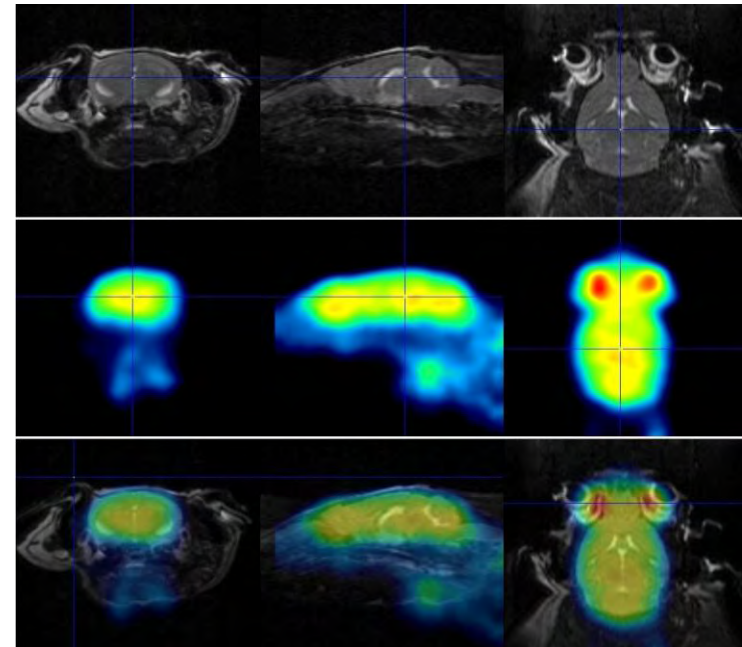
## Metabolic Changes in Alzheimer's Models



### Control



### APP+



Prof. M.A.Pozo Instituto Pluridisciplinar. Universidad Complutense de Madrid

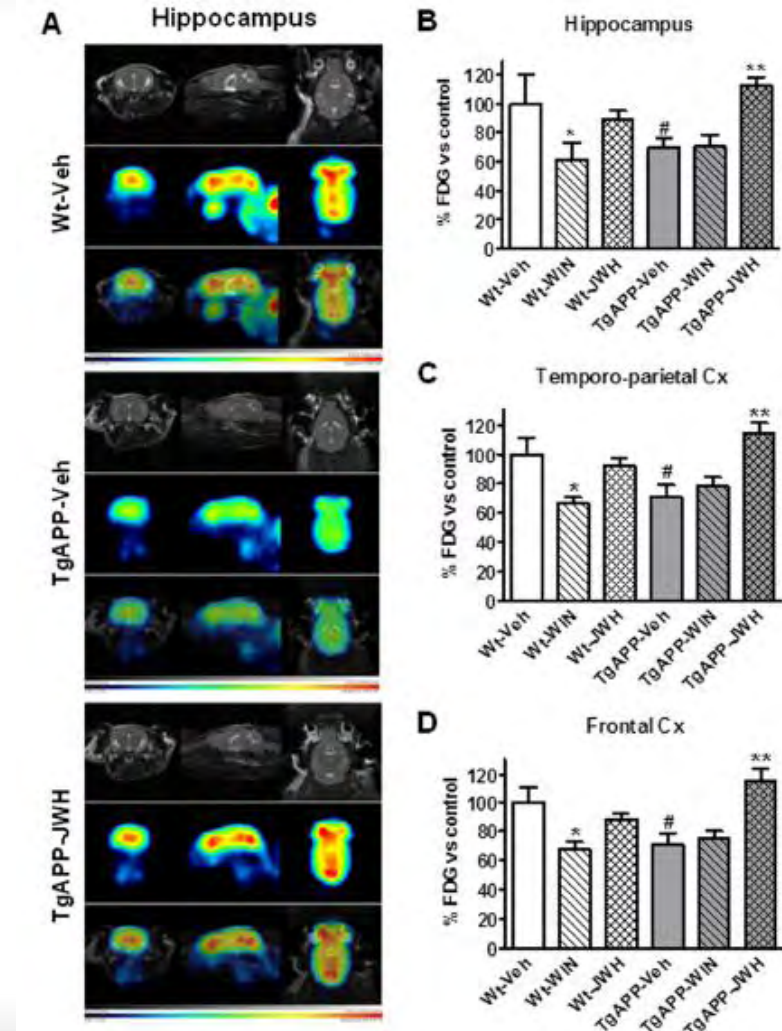
- significant decrease in brain metabolism in mouse models that over express APP
- can be readily visualized with the Albira system and then in this case co-registered with T2 weighted MRI images
- Co-registration done using the supplied PMOD software package and MRI compatible animal transport beds. Animals were imaged with  $^{18}\text{F}$ -FDG



# Positron Emission Tomography

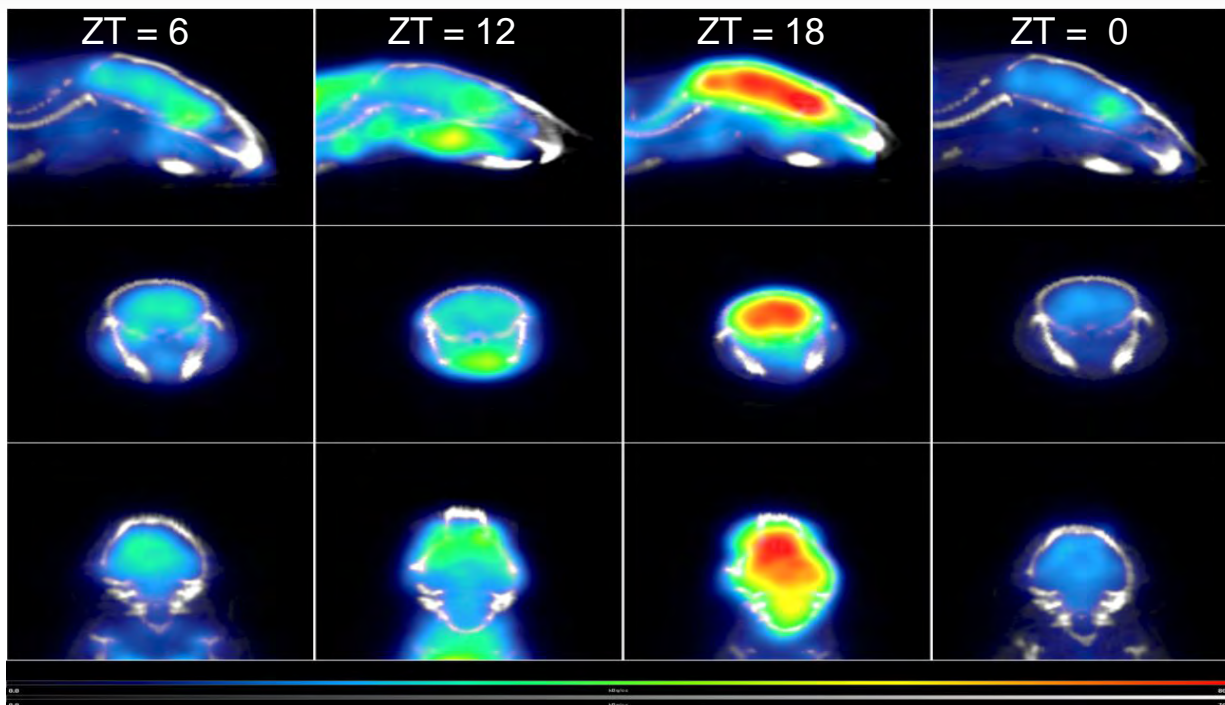
A $\beta$  Damage reduced by Cannabinoids –  $^{18}\text{F}$ -FDG PET

- App Tg mice show decreased levels of FDG Uptake
- Treatment with CB2 selective agonist JWH rescued glucose metabolism reduction
- CB<sub>2</sub> agonist also rescued behavioral deficits
- Note: CB<sub>1</sub> activation induces psychoactive effects NOT CB<sub>2</sub> activation



# Positron Emission Tomography

Effects of circadian rhythm on brain metabolism –  $^{18}\text{F}$ -FDG PET/CT



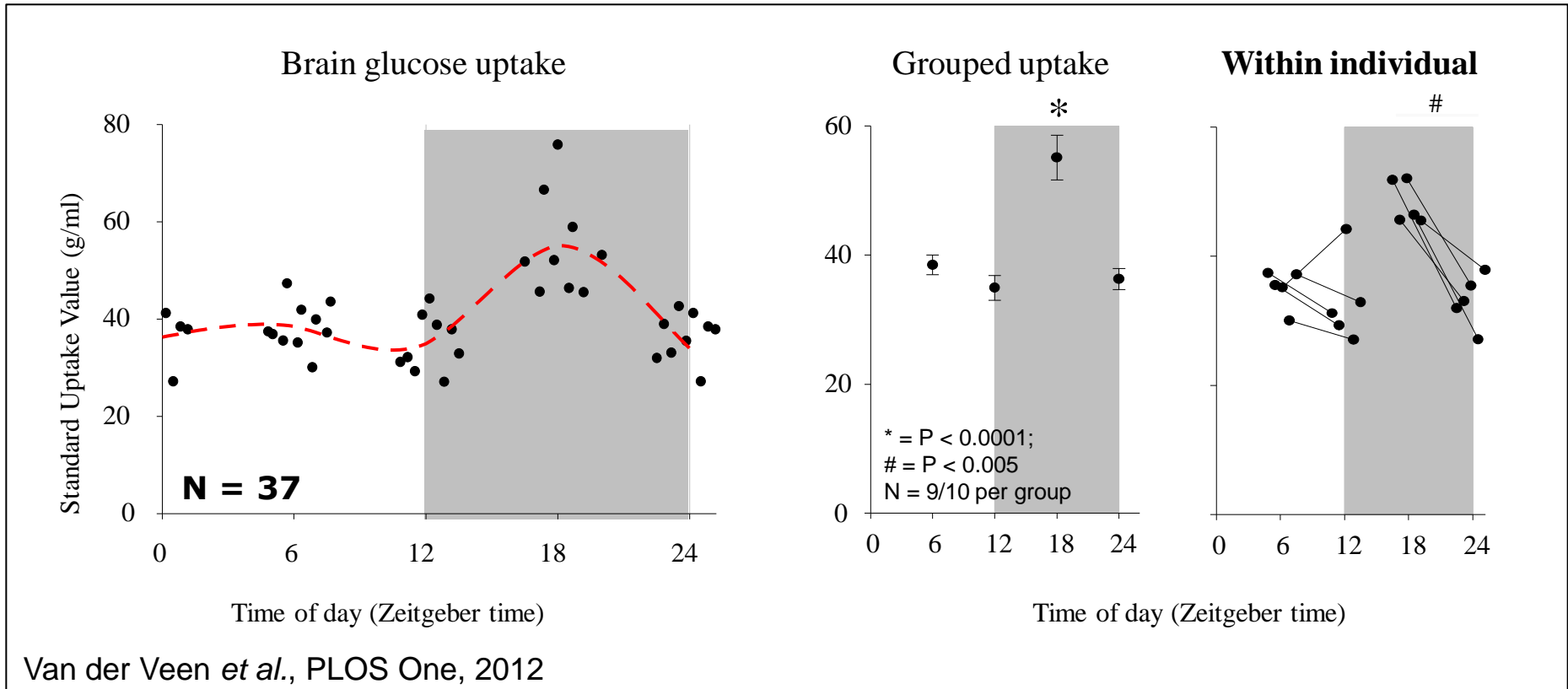
Dr. Daan van der Veen and graduate student Jinping Shou, from the laboratory of Prof. Giles Duffield, are measuring the effects of circadian rhythms on brain metabolism using *in vivo* PET-CT imaging.

In both whole brain but not in sub brain regions you can observe circadian rhythms in the murine brain with peak activity in the night time. ZT means Zeitgeber time which is a normalized day night cycle.



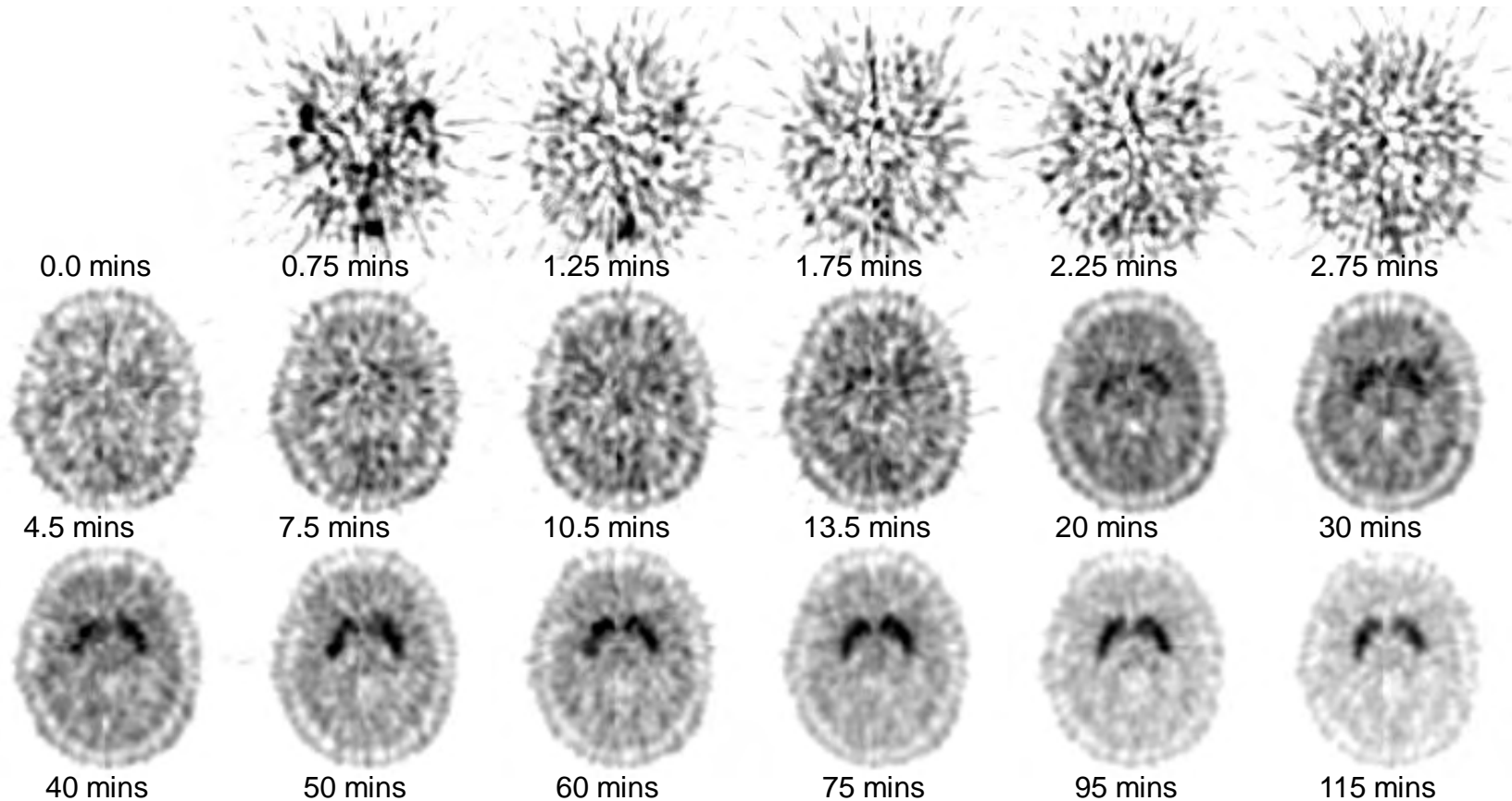
# Positron Emission Tomography

Effects of circadian rhythm on brain metabolism –  $^{18}\text{F}$ -FDG PET/CT



# Positron Emission Tomography

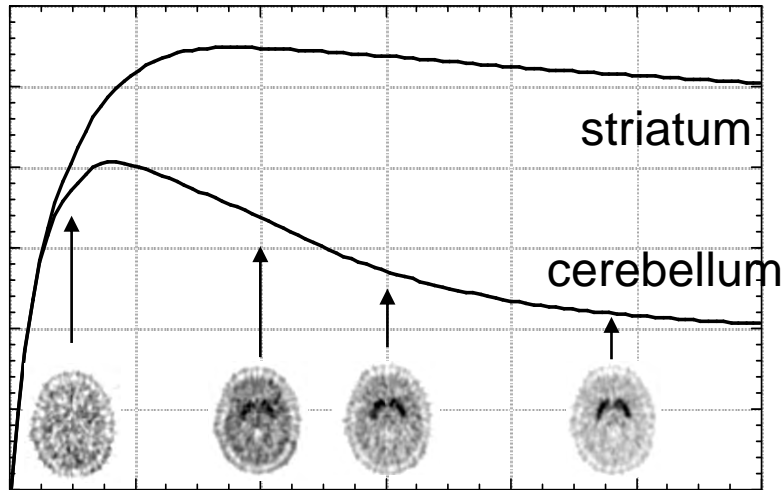
$^{18}\text{F}$ -FDOPA time course in mouse brain



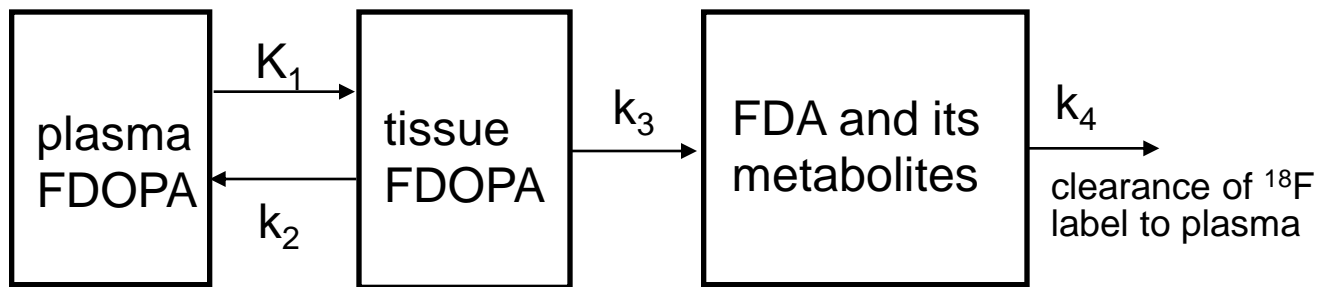
Crump Institute for Biological Imaging, UCLA

# Positron Emission Tomography

## $^{18}\text{F}$ -FDOPA - Tracer Kinetic Modeling



- Simplified model for FDOPA kinetics in striatum
- Rate constants  $K_1$ ,  $k_2$ ,  $k_3$  &  $k_4$  can be estimated using measured PET time activity curves and blood input function.



FDOPA = [ $^{18}\text{F}$ ]fluoroDOPA

Crump Institute for Biological Imaging, UCLA



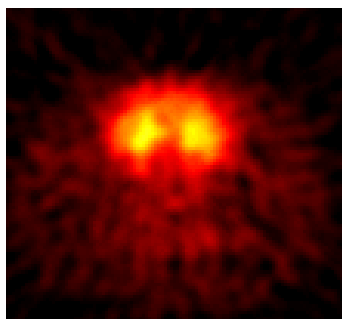


# Positron Emission Tomography

## Striatal Dopamine System of Rats

[C-11]WIN 35,428

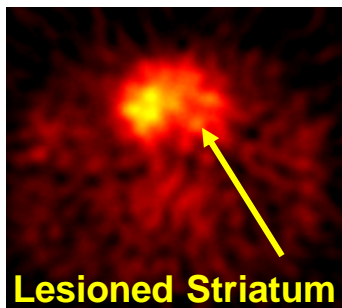
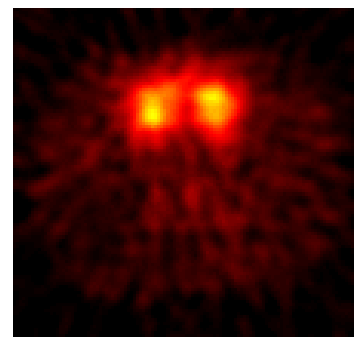
DA Transporter Binding



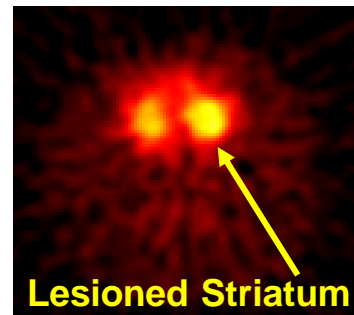
Control

[C-11]Raclopride

DA D2 Receptor Binding



Unilateral  
6-Hydroxydopamine  
Lesion



Dan Rubins, Goran Lacan, Simon Cherry, and William Melega

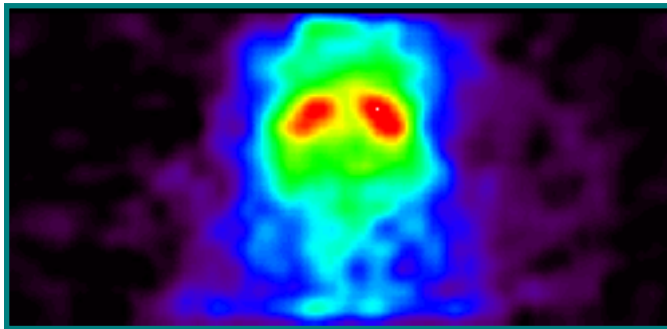


# Positron Emission Tomography

$^{11}\text{C}$ -WIN 35, 428 in mouse brain

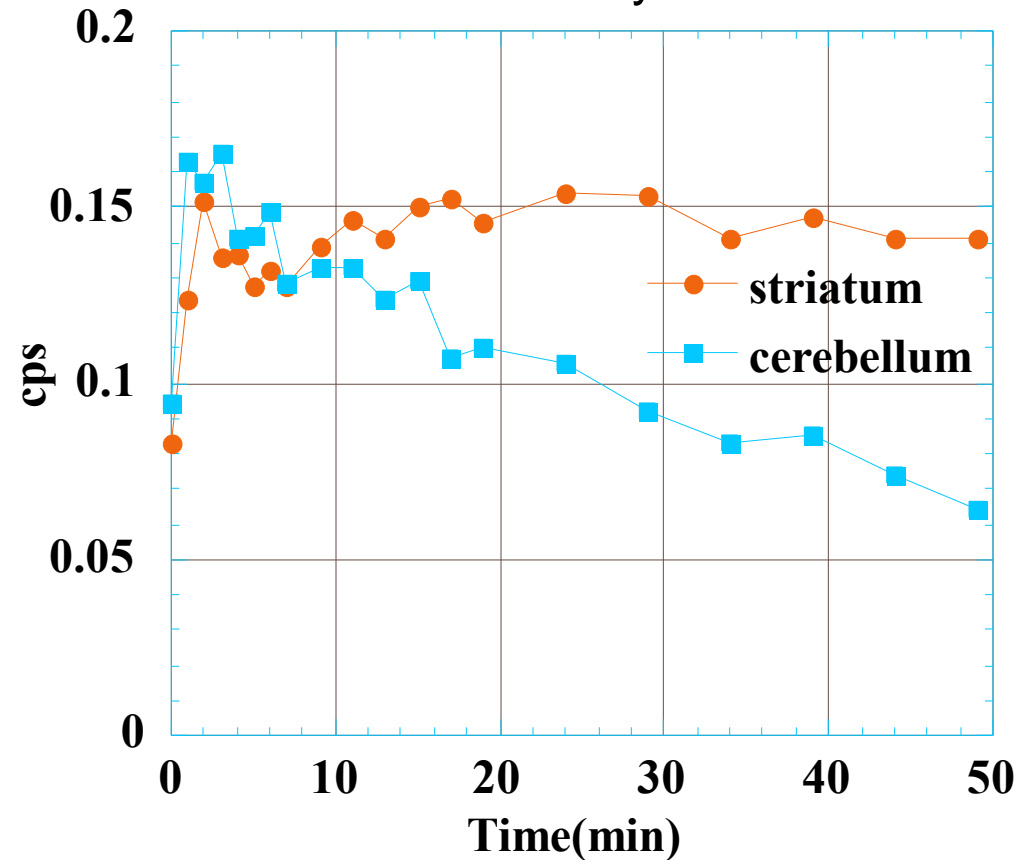


30g mouse  
transverse brain section



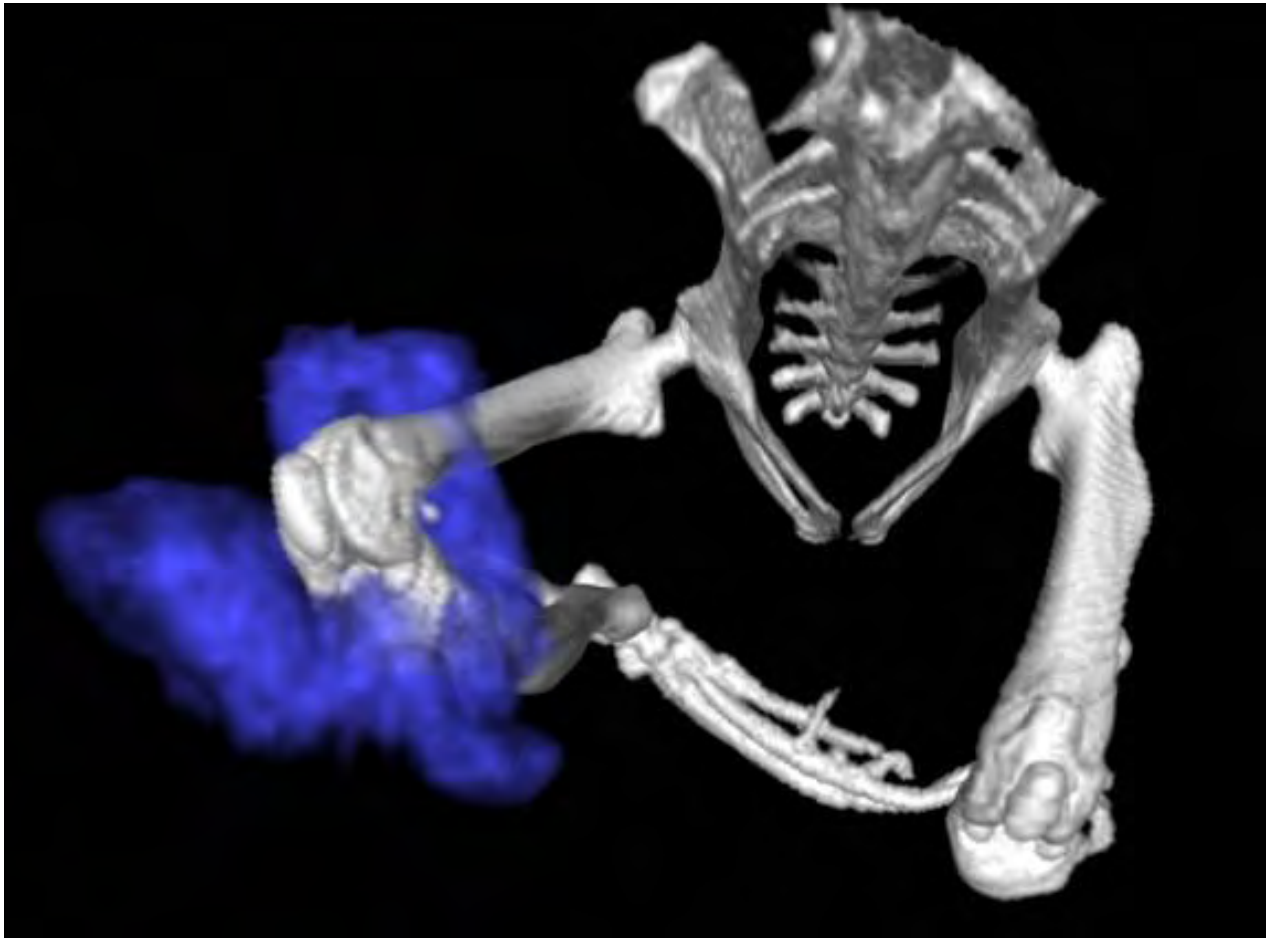
180  $\mu\text{Ci}$  of  $^{11}\text{C}$ -WIN 35,428  
(0.018  $\mu\text{g}$ )

Time Activity curve



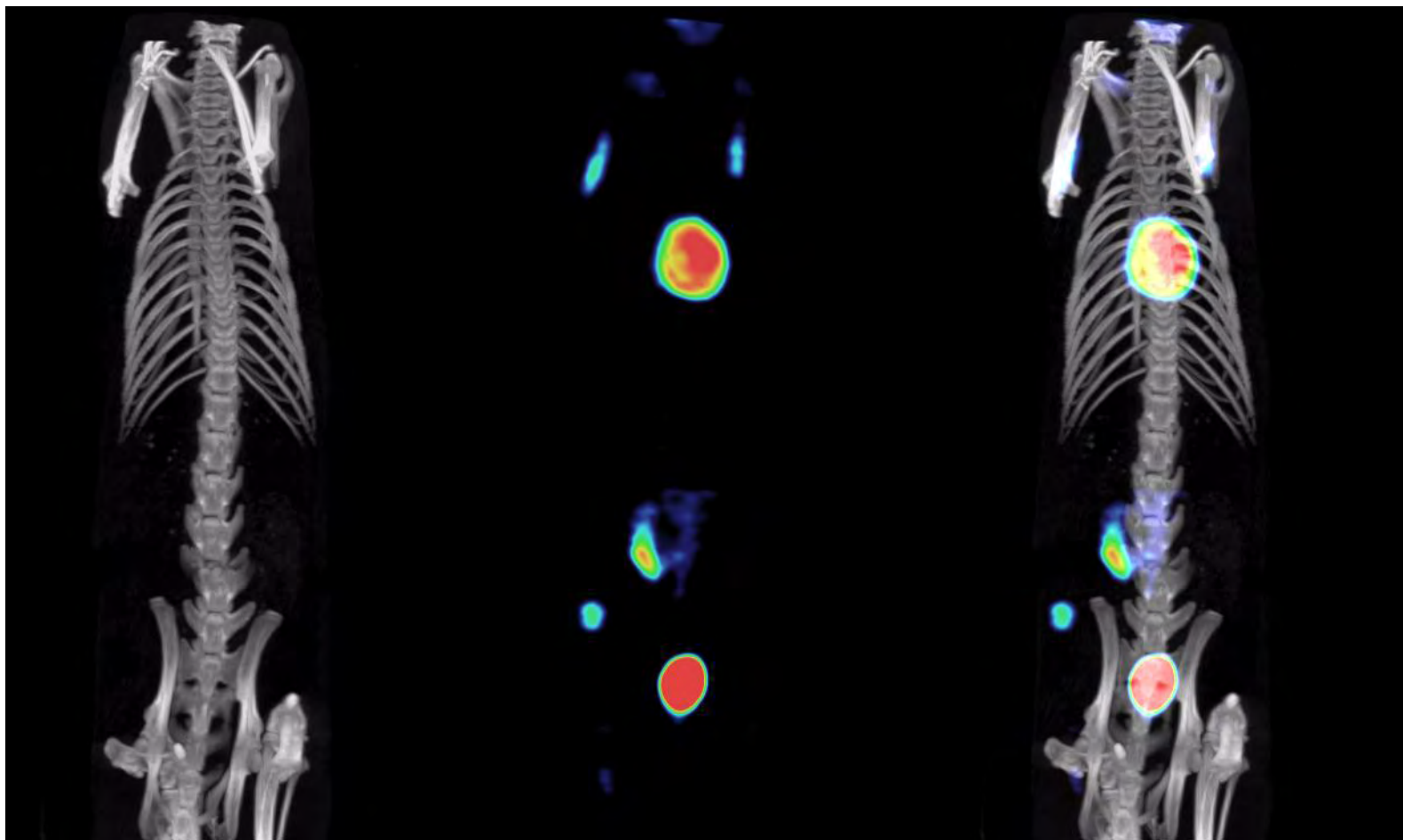
# Positron Emission Tomography

Oncology & Therapeutic Evaluation



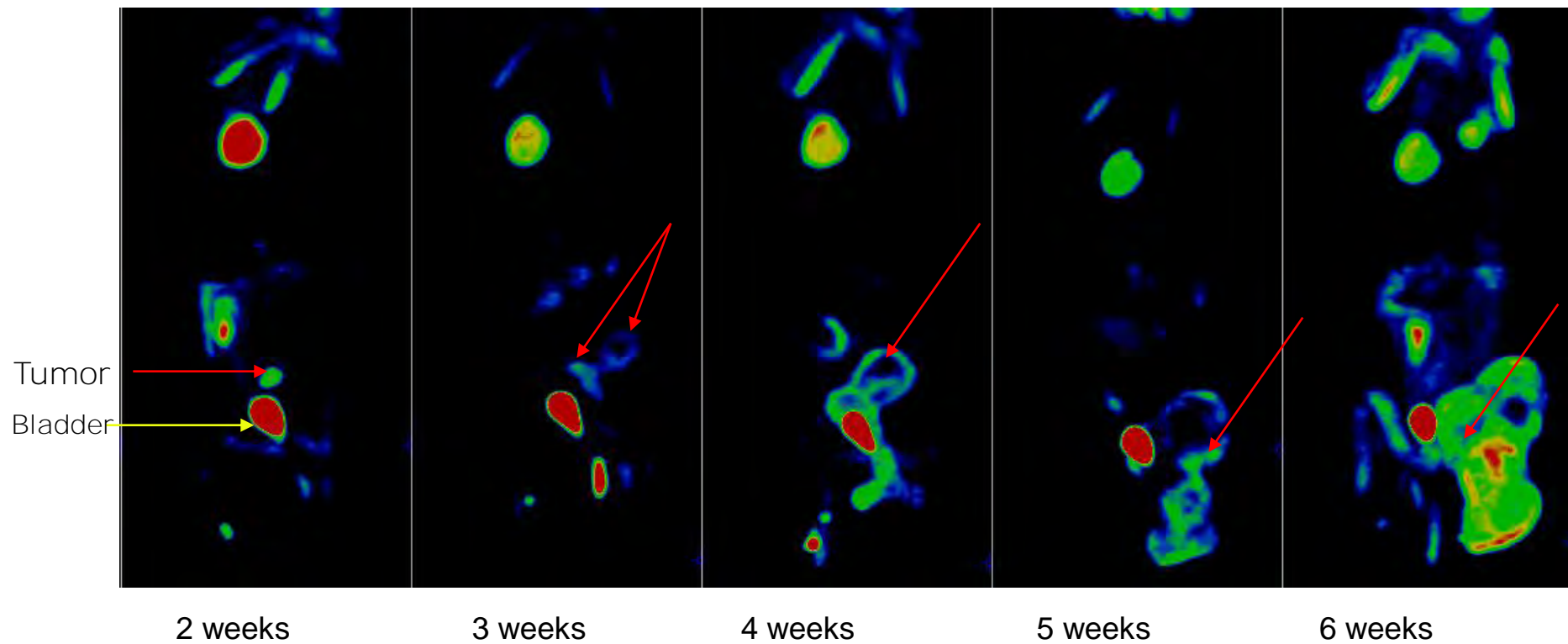
# Positron Emission Tomography

Colon Cancer Xenograft –  $^{18}\text{F}$ -FDG PET/CT



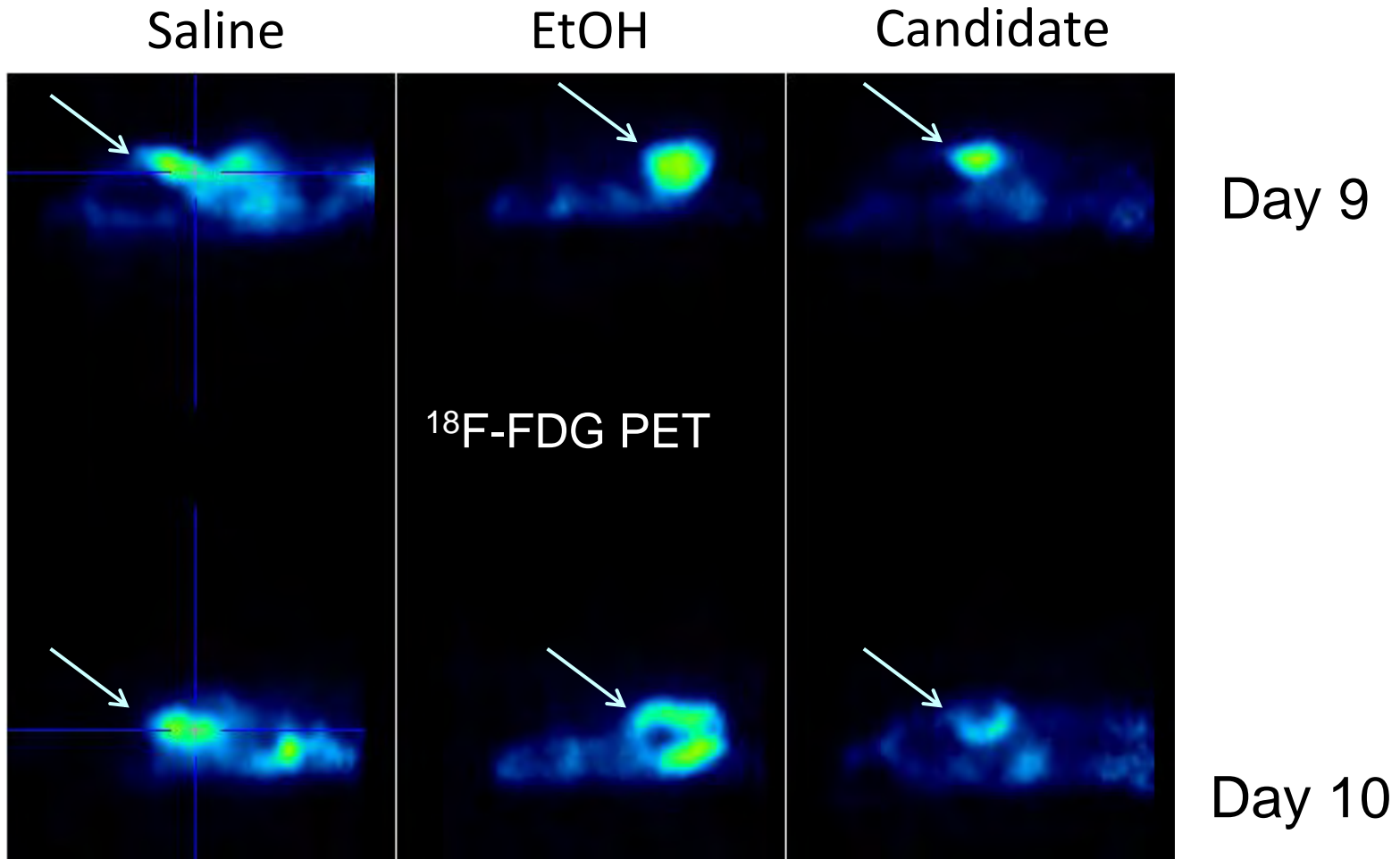
# Positron Emission Tomography

Colon Cancer Xenograft –  $^{18}\text{F}$ -FDG PET – 6 week progression



# Positron Emission Tomography

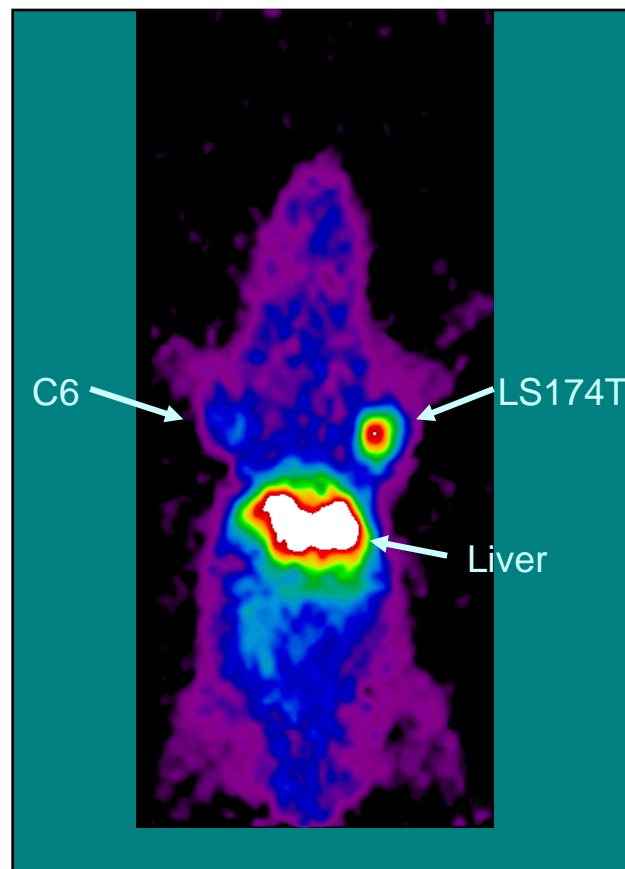
Evaluation of locoregional application of chemotherapeutics



# Positron Emission Tomography

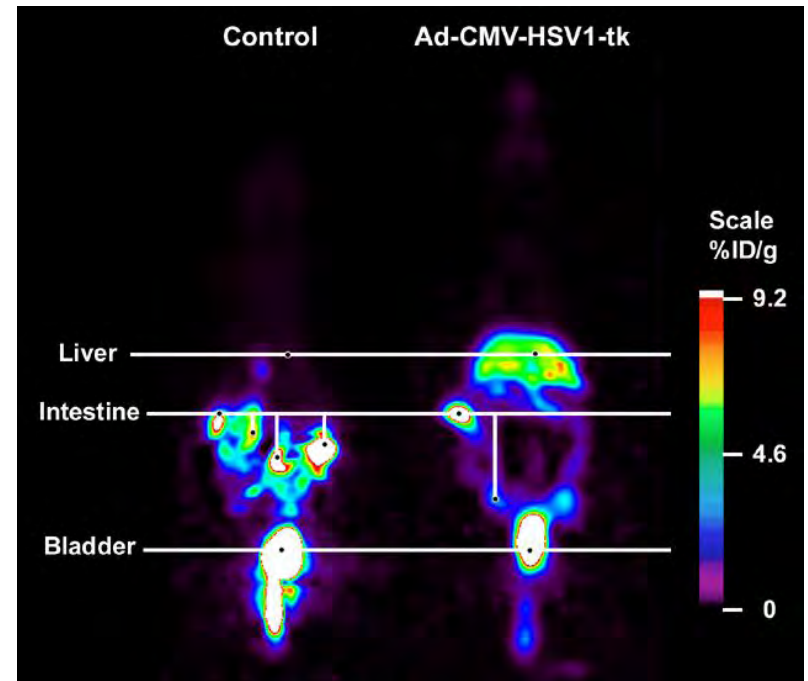
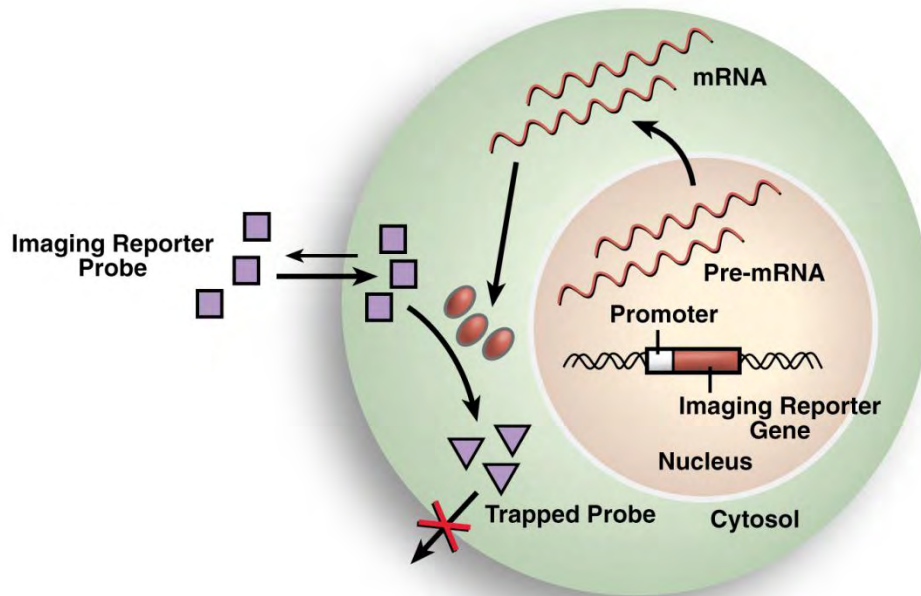
$^{64}\text{Cu}$ -DOTA anti-CEA Minibody

- Athymic mouse with LS174T (CEA+) and C6 (CEA-) xenografts
- Injected with  $70\ \mu\text{Ci}$   $^{64}\text{Cu}$ -anti-CEA minibody (engineered antibody fragment, scFv- $\text{C}_{\text{H}3}$ )
- Scanned 12 hr post injection
- Courtesy of Anna Wu (UCLA and City of Hope)



# Positron Emission Tomography

Imaging gene Expression by PET



Crump Institute for Biological Imaging, UCLA





# Positron Emission Tomography

microPET in Drug Development

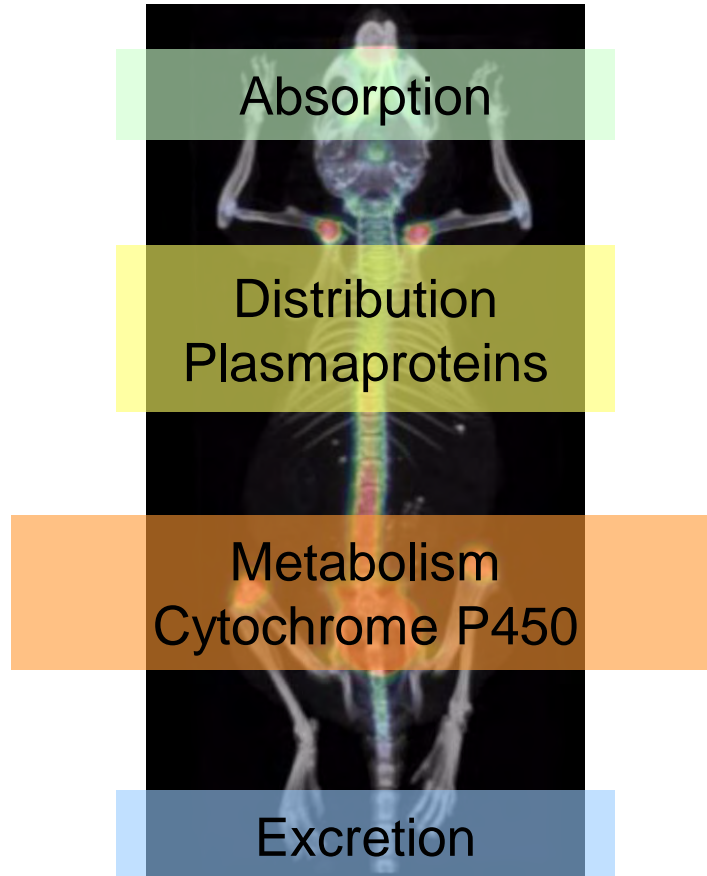


- direct radiolabeling of drug
  - biodistribution and pharmacokinetics
- binding/competition studies
  - dosing and pharmacodynamics
- indirect markers
  - pharmacodynamic effect on secondary marker (e.g. metabolism or blood flow)



# Pharmacokinetic

A<sub>bsorption</sub>; D<sub>istribution</sub>, M<sub>etabolism</sub>, E<sub>xcretion</sub>





# Radiopharmacy

Routine Production, Custom Synthesis & Labeling Concepts



**Nuclear Physics Institute of the Academy of Sciences of the Czech Republic, p.r.i.  
Department of Radiopharmaceuticals**



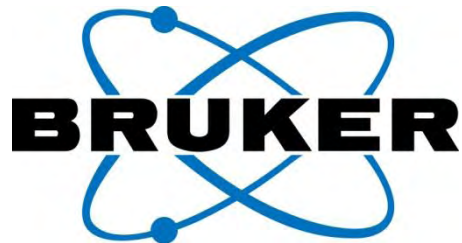
**Ass. Prof. Ondřej Lebeda, Ph.D.**

Head of Department

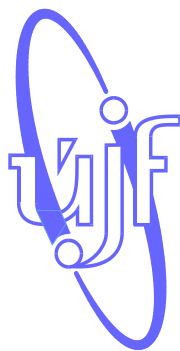
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# Thank You



## for Your Attention